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NEURORECEPTOR AVAILABILITY AND CEREBRAL MORPHOLOGY IN HUMAN OBESITY

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Were I a physician with a diploma, I would have written a whole book on obesity; thus I would have acquired a domicile in the domain of science, and would have had the double satisfaction of having, as patients, persons who were perfectly well, and of being besieged by the fairer portion of humanity. —
What I have not done, some other person will do, and if he be learned and prudent (and at the same time a good-fellow), I foretell that he will have wonderful success.

-Jean Anthelme Brillat-Savarin,
La Physiologie du Goût, translated by Fayette Robinson

Isn't it funny
How a bear likes honey?
Buzz! Buzz! Buzz!
I wonder why he does?

-A. A. Milne, *Winnie the Pooh*

To Kerttu and Väinö

ABSTRACT

Henry Karlsson

Neuroreceptor availability and cerebral morphology in human obesity

University of Turku, Faculty of Medicine, Department of Neurology; University of Turku Doctoral Programme of Clinical Investigation and The National Graduate School of Clinical Investigation; Turku PET Centre, University of Turku and Turku University Hospital

Obesity is a major challenge to human health worldwide. Little is known about the brain mechanisms that are associated with overeating and obesity in humans. In this project, multimodal neuroimaging techniques were utilized to study brain neurotransmission and anatomy in obesity. Bariatric surgery was used as an experimental method for assessing whether the possible differences between obese and non-obese individuals change following the weight loss. This could indicate whether obesity-related altered neurotransmission and cerebral atrophy are recoverable or whether they represent stable individual characteristics.

Morbidly obese subjects (BMI ≥ 35 kg/m²) and non-obese control subjects (mean BMI 23 kg/m²) were studied with positron emission tomography (PET) and magnetic resonance imaging (MRI). In the PET studies, focus was put on dopaminergic and opioidergic systems, both of which are crucial in the reward processing. Brain dopamine D₂ receptor (D₂R) availability was measured using [¹¹C]raclopride and μ -opioid receptor (MOR) availability using [¹¹C]carfentanil. In the MRI studies, voxel-based morphometry (VBM) of T1-weighted MRI images was used, coupled with diffusion tensor imaging (DTI). Obese subjects underwent bariatric surgery as their standard clinical treatment during the study.

Preoperatively, morbidly obese subjects had significantly lower MOR availability but unaltered D₂R availability in several brain regions involved in reward processing, including striatum, insula, and thalamus. Moreover, obesity disrupted the interaction between the MOR and D₂R systems in ventral striatum. Bariatric surgery and concomitant weight loss normalized MOR availability in the obese, but did not influence D₂R availability in any brain region.

Morbidly obese subjects had also significantly lower grey and white matter densities globally in the brain, but more focal changes were located in the areas associated with inhibitory control, reward processing, and appetite. DTI revealed also signs of axonal damage in the obese in corticospinal tracts and occipito-frontal fascicles. Surgery-induced weight loss resulted in global recovery of white matter density as well as more focal recovery of grey matter density among obese subjects.

Altogether these results show that the endogenous opioid system is fundamentally linked to obesity. Lowered MOR availability is likely a consequence of obesity and may mediate maintenance of excessive energy uptake. In addition, obesity has adverse effects on brain structure. Bariatric surgery however reverses MOR dysfunction and recovers cerebral atrophy. Understanding the opioidergic contribution to overeating and obesity is critical for developing new psychological or pharmacological treatments for obesity. The actual molecular mechanisms behind the positive change in structure and neurotransmitter function still remain unclear and should be addressed in the future research.

Key words: bariatric surgery, diffusion tensor imaging, dopamine, magnetic resonance imaging, obesity, opioids, positron emission tomography, reward circuit, voxel-based morphometry

TIIVISTELMÄ

Henry Karlsson

Neuroreseptorit ja aivojen rakenne lihavuudessa

Turun yliopisto, Lääketieteellinen tiedekunta, Neurologian laitos; Turun yliopiston kliininen tohtorihjelma ja Valtakunnallinen kliininen tutkijakoulu; Valtakunnallinen PET-keskus, Turun yliopisto ja Turun yliopistollinen keskussairaala

Lihavuudesta on tullut yksi maailman suurimmista terveysongelmista. Lihavuuteen liittyvistä aivojen toiminnan ja rakenteen muutoksista tiedetään kuitenkin toistaiseksi melko vähän. Tässä tutkimuksessa selvitettiin aivojen välittäjäainetoiminnan ja rakenteen eroja lihavien ja normaali-painoisten henkilöiden välillä. Lihavuusleikkauksen ja sitä seuraavan laihtumisen aiheuttamia aivojen välittäjäainetoiminnan ja tiheyden muutoksia arvioimalla voitiin päätellä, ovatko aivomuutokset jo olemassa ennen lihavuuden syntyä vai ovatko ne lihavuuden aiheuttamia.

Vaikeasti lihavien henkilöiden ($BMI \geq 35 \text{ kg/m}^2$) aivoja verrattiin normaalipainoisten henkilöiden (BMI :n keskiarvo 23 kg/m^2) aivoihin käyttämällä positroniemissiotomografiaa (PET) ja magneettiresonanssikuvantamismenetelmiä (MRI). PET-tutkimuksissa käytettiin kahta radioisotoopilla leimattua merkkiainetta, joista [^{11}C]raklopridi sitoutuu dopamiinin D_2 -reseptoreihin ja [^{11}C]karfentaniili μ -opioidireseptoreihin. Kummatkin reseptorit ovat keskeisessä asemassa aivojen mielihyväjärjestelmän toiminnassa. MRI-tutkimuksissa käytettiin analyysimenetelminä vokselipohjaista morfometriä (*voxel-based morphometry*, VBM) sekä diffuusiotensorikuvantamista (*diffusion tensor imaging*, DTI). Lihaville tutkittaville tehtiin tutkimuksen aikana lihavuusleikkauksen aikaisemman hoitosuunnitelman mukaisesti.

Ennen lihavuusleikkausta lihavilla tutkittavilla oli selvästi vähemmän μ -opioidireseptoreja mielihyväjärjestelmän keskeisissä osissa, kuten tyvitumakkeissa, insulassa ja talamuksessa, mutta dopamiinin D_2 -reseptorien määrä oli sama kuin normaalipainoisilla tutkittavilla. Lisäksi näiden reseptorijärjestelmien välinen yhteys oli häiriintynyt lihavilla tutkittavilla aivojuovion etuosassa. Lihavuusleikkauksen aiheuttaman laihtumisen jälkeen μ -opioidireseptorien määrä palautui samalle tasolle kuin normaalipainoisilla. Dopamiinireseptorien määrässä ei tapahtunut muutosta.

Magneettitutkimuksissa kävi ilmi, että lihavilla tutkittavilla aivojen harmaan ja valkean aineen tiheydet olivat pienemmät kuin normaalipainoisilla tutkittavilla. Eroa löytyi erityisesti mielihyvään ja ruokahaluuun liittyvillä alueilla. Myös valkean aineen radastoissa oli vaurion merkkejä. Leikkauksen jälkeen tapahtui palautumista laajasti valkean aineen alueilla mutta myös selvästi pienemmillä harmaan aineen alueilla.

Tulokset osoittavat, että opioidijärjestelmä liittyy keskeisesti lihavuuteen ja liikasyömiseen. Opioidijärjestelmän poikkeava toiminta on todennäköisesti lihavuuden aiheuttamaa ja saattaa ylläpitää haitallista syömiskäyttäytymistä. Lisäksi lihavuudella on haitallisia vaikutuksia aivojen rakenteeseen. Lihavuusleikkaus palauttaa opioidijärjestelmän ennalleen ja korjaa lihavuuden aiheuttamaa aivokudoksen harventumaa. Opioidijärjestelmän merkityksen ymmärtäminen on välttämätöntä lihavuuden uusien psykologisten ja farmakologisten hoitomuotojen kehittämisessä. Solutuksen mekanismit leikkauksen aiheuttamien muutosten taustalla ovat kuitenkin edelleen epäselvät, ja niihin tulisi keskittyä jatkotutkimuksissa.

Avainsanat: diffuusiotensorikuvantaminen, dopamiini, lihavuus, lihavuusleikkaus, magneettiresonanssikuvantaminen, mielihyväjärjestelmä, opioidit, positroniemissiotomografia, vokselipohjainen morfometria

TABLE OF CONTENTS

ABBREVIATIONS	8
LIST OF ORIGINAL PUBLICATIONS	10
1 INTRODUCTION.....	11
2 REVIEW OF THE LITERATURE	12
2.1 Cerebral regulation of appetite.....	12
2.2 Obesity and the reward circuit	13
2.2.1 <i>Reward systems in the human brain.....</i>	<i>13</i>
2.2.2 <i>Dopaminergic system in reward functions and obesity</i>	<i>13</i>
2.2.3 <i>Endogenous opioid system in human reward and obesity</i>	<i>15</i>
2.2.4 <i>Interaction between dopaminergic and opioidergic systems in obesity.....</i>	<i>16</i>
2.2.5 <i>Is obesity an addictive disorder?.....</i>	<i>16</i>
2.3 Obesity and brain atrophy	18
2.4 Does weight loss alter brain function and structure?.....	19
2.5 Summary of the literature	20
3 OBJECTIVES OF THE STUDY.....	21
4 GENERAL METHODOLOGY.....	22
4.1 Subjects	22
4.2 Overall study design.....	23
4.3 Positron Emission Tomography (PET).....	24
4.3.1 <i>PET image acquisition (Studies I-III)</i>	<i>25</i>
4.3.2 <i>PET data analysis (Studies I-III).....</i>	<i>26</i>
4.4 Magnetic Resonance Imaging (MRI).....	28
4.4.1 <i>MR Image acquisition (Studies I-V)</i>	<i>29</i>
4.4.2 <i>VBM data analysis (Studies IV-V).....</i>	<i>30</i>
4.4.3 <i>DTI data analysis (Study IV)</i>	<i>30</i>
5 RESULTS	32
5.1 Obesity is associated with decreased cerebral MOR availability (Study I)	32
5.2 Interaction between dopamine and opioid systems is disrupted in morbid obesity (Study II).....	33
5.3 Bariatric surgery and weight loss normalizes MOR availability in morbid obesity (Study III).....	34
5.4 Obesity is linked to cerebral atrophy and decreased white matter integrity (Study IV)	35
5.5 Bariatric surgery and weight loss recovers GM and WM atrophy in morbid obesity (Study V).....	37

6	DISCUSSION	40
6.1	Obesity is associated with opioidergic dysfunction	40
6.2	Bariatric surgery and weight loss recovers the opioidergic dysfunction in the brain reward circuit.....	41
6.3	Obesity has a profound impact on brain anatomy and integrity but this is reversed after bariatric surgery	43
6.4	Clinical implications.....	44
6.5	Limitations of the studies	46
6.6	Future directions	47
7	CONCLUSIONS	49
8	ACKNOWLEDGEMENTS	50
9	REFERENCES	53
	ORIGINAL PUBLICATIONS	65

ABBREVIATIONS

BDI-II = Beck Depression Inventory II

BMI = body mass index

BP_{ND} = binding potential (non-displaceable uptake)

CCK = cholecystokinin

CT = computed tomography

D₂R = dopamine D₂ receptor

DAT = dopamine transporter

DEBQ = Dutch Eating Behaviour Questionnaire

DTI = diffusion tensor imaging

DW = diffusion-weighted

EPI = echo-planar imaging

FA = fractional anisotropy

FCQ = Food Craving Questionnaire

FDR = false discovery rate

fMRI = functional magnetic resonance imaging

FWE = family wise error

FWHM = full width at half maximum

GLM = general linear model

GLP-1 = glucagon like peptide 1

GM = gray matter

HDL = high density lipoprotein

LOR = line of response

MD = mean diffusivity

MNI = Montreal Neurological Institute

MOR = μ -opioid receptor

MR = magnetic resonance

MRI = magnetic resonance imaging

OGTT = oral glucose tolerance test

PET = positron emission tomography

PYY = peptide-YY

ROI = region of interest

RYGB = Roux-en-Y gastric bypass operation

SD = standard deviation

SAT = subcutaneous adipose tissue

SPECT = single-photon emission computed tomography

SPM = statistical parametric mapping

SRTM = simplified reference tissue model

STAI = State-Trait Anxiety Inventory

TAC = time-activity curve

TE = echo time

TR = repetition time

VAT = visceral adipose tissue

VBM = voxel based morphometry

VTA = ventral tegmental area

WM = white matter

YFAS = Yale Food Addiction Scale

LIST OF ORIGINAL PUBLICATIONS

This thesis is based on the following original publications, which are referred to in the text by the Roman numerals I-V:

I **Karlsson HK**, Tuominen L, Tuulari JJ, Hirvonen J, Parkkola R, Helin S, Salminen P, Nuutila P and Nummenmaa L. 2015. Obesity is associated with decreased μ -opioid but unaltered dopamine D2 receptor availability in the brain. *The Journal of Neuroscience* 35:3959-65.

II Tuominen L, Tuulari JJ, **Karlsson HK**, Hirvonen J, Helin S, Parkkola R, Salminen P, Hietala J, Nuutila P and Nummenmaa L. 2015. Aberrant mesolimbic dopamine-opiate interaction in obesity. *Neuroimage* 122:80-86.

III **Karlsson HK**, Tuulari JJ, Tuominen L, Hirvonen J, Honka H, Parkkola R, Helin S, Salminen P, Nuutila P and Nummenmaa L. 2015. Weight loss after bariatric surgery normalizes brain opioid receptors in morbid obesity. *Molecular Psychiatry* (epub Oct 13).

IV **Karlsson HK**, Tuulari JJ, Hirvonen J, Lepomäki V, Parkkola R, Hiltunen J, Hannukainen JH, Soinio M, Pham T, Salminen P, Nuutila P and Nummenmaa L. 2013. Obesity is associated with white matter atrophy: a combined diffusion tensor imaging and voxel-based morphometric study. *Obesity* 21:2530-7.

V Tuulari JJ, **Karlsson HK**, Antikainen O, Hirvonen J, Pham T, Salminen P, Helmiö M, Parkkola R, Nuutila P and Nummenmaa L. Bariatric surgery induces white and grey matter density recovery in the morbidly obese: A voxel-based morphometric study. *Human Brain Mapping* (accepted).

The original articles (I – V) have been reproduced with the permission of the publishers.

1 INTRODUCTION

Obesity is an immense burden to human health and economy worldwide. The prevalence of obesity has increased steeply over the last decades. In Finland, 20 % of the adult population is obese (Männistö et al., 2012), while in the United States percentage is over 30 % (Ogden et al., 2014). There are no signs of termination of the obesity epidemic. Quite the contrary: we live in a highly “obesogenic” environment, where physical, social, and cultural factors make many people to eat more than they need to in order to survive. Therefore, the enormous public and personal health costs caused by obesity and its comorbidities will rise in the future. According to the recent statistics of World Health Organization, more than 2.8 million people die each year because of overweight and obesity (WHO, 2015). Increase of mortality originates from the numerous harmful metabolic effects associated with increased body weight, including elevated blood pressure and insulin resistance. Thus, obesity is linked to numerous co-morbidities such as hypertension, type 2 diabetes, and coronary heart disease.

Several studies have tried to reveal the causes of obesity. It is now obvious that common obesity is a complex, multifactorial, and heterogenous condition, which cannot be explained by, for example, simple genetic factors, although few exceptions may exist (Albuquerque et al., 2015). While the adverse effects of obesity to internal organs are well described, growing evidence shows that obesity is also associated with changes in brain morphology and function. Moreover, it is possible that individual differences in brain networks subserving reward processing and appetite control may make some individuals prone to weight gain. Studies have shown reductions in gray matter density in obese versus normal-weight individuals, and some studies have pointed out changes in white matter as well. There are also studies that have found neurochemical alterations in obesity. Some researchers have even drawn parallels between obesity and addictive disorders, mainly because the hallmark of many addictive disorders – lowered dopamine D₂ receptor (D₂R) density in the striatum – has been observed in obese individuals. Animal studies also highlight the importance of endogenous opioid system, particularly the μ -opioid receptor (MOR), in eating and obesity, but currently its role in human obesity remains unresolved. Furthermore, it is currently unknown whether cerebral atrophy and altered neurotransmission are causes or consequences of obesity.

Identifying the neurochemical mechanisms that make some individuals prone to overeating as well as pinpointing how obesity changes the functioning and the anatomy of the human brain is critical for understanding the current high prevalence of obesity and designing appropriate therapies for obesity. In the experimental studies presented in this thesis, a multimodal neuroimaging techniques including positron emission tomography (PET), diffusion tensor imaging (DTI), and voxel-based morphometry (VBM), were used to study brain function and anatomy in morbidly obese and normal-weight individuals. Obese subjects underwent bariatric surgery, which is so far the most efficient way of losing weight and remitting co-morbid diseases such as diabetes. This allowed evaluating whether the observed differences between obese and normal-weight individuals are recoverable by weight loss, or whether they represent stable traits in obesity.

2 REVIEW OF THE LITERATURE

2.1 Cerebral regulation of appetite

Animals depend solely on food as their source of energy. Consequently, feeding has to be secured to offer optimal possibilities for survival. In normal conditions, food intake and the choice of food is controlled by the mesocorticolimbic areas of the brain, including hypothalamus, striatum, amygdala, and prefrontal cortices. Hypothalamus constitutes the key part of physiological appetite regulation in the brain. It receives neural and humoral signals from the other parts of body, and integrates these signals together with insula in order to keep the body weight in balance (Saper et al., 2002; Berthoud, 2012). Most important gut hormones associated with appetite control are glucagon-like peptide 1 (GLP-1), peptide-YY (PYY), ghrelin, and cholecystokinin (CCK). Hypothalamus also sensors body adiposity via leptin, a hormone produced by adipose cells (Keen-Rhinehart et al., 2013) and an important factor in the control of feeding and energy expenditure in humans (Ahima, 2008).

Homeostatic mechanisms form the basis of appetite control, yet they are supported by brain's reward circuit, which guides appetitive motivation and generation of pleasurable sensations upon food consumption. Common obesity does not originate from dysfunctional homeostatic mechanisms only, and the brain systems controlling pleasure and reward are also critical for overeating and obesity (Kringelbach, 2004; Berthoud, 2012; Keen-Rhinehart et al., 2013; Alonso-Alonso et al., 2015; Yu et al., 2015). Feeding has a strong hedonic aspect, and both humans and animals can eat for the sake of pleasure regardless of current energy balance (Palmiter, 2007; Kenny, 2011; Johnson, 2013). Moreover, volitional appetite control is partly impaired among obese subjects, which may cause unhealthy eating patterns (Batterink et al., 2010; Tuulari et al., 2015).

In the modern western society where continuous flow of food and food product imagery are served to people, the role of actual physiological control of appetite may become less important. It is likely that the dysfunction of reward circuit and volitional appetite control are possible culprits behind the obesity epidemic. Additionally, integration of homeostatic control and reward functions play a pivotal role in the onset of pathological eating habits. For example, animal studies have shown a direct link between leptin and dopaminergic system, as leptin seems to inhibit the reward circuit through dopaminergic neurons (Fulton et al., 2006; Hommel et al., 2006). Also insulin and ghrelin can directly interact with dopaminergic system (Kenny, 2011; Dunn et al., 2012).

2.2 Obesity and the reward circuit

2.2.1 *Reward systems in the human brain*

Multiple reward systems are located in the mammalian brain (Kringelbach, 2004). Based on wide range of studies, the distinction between neuronal circuits for reward *wanting* and *liking* has been made. Wanting is a process of incentive motivation, which directs behaviour towards obtaining certain goals, whereas liking refers to the hedonic reaction to the pleasure associated with reward consumption. Although these processes are highly related, they remain dissociable. (Berridge, 2009; Castro and Berridge, 2014; Berridge and Kringelbach, 2015). For a long time, dopamine was regarded as the major neurotransmitter in reward and pleasure, but recent evidence has shown that mesolimbic dopamine neurons may be more important in motivational drive, such as wanting and craving, and the actual pleasure response may have other contributors. In contrast to dopaminergic system, the opioidergic system has been more consistently linked with hedonic responses and 'liking' responses. Both wanting and liking functions as well as the systems subserving them – dopaminergic and opioidergic systems, respectively – are needed for normal reward (Berridge, 2009; Berridge et al., 2010; Berridge and Kringelbach, 2015).

Several animal and human studies have confirmed that the reward system is dysfunctional in obesity. Overeating is considered to originate from the imbalance between the reward circuit involving ventral striatum, amygdala, and several other interconnected brain regions, and the regions that inhibit reward-seeking such as dorsolateral prefrontal and orbitofrontal cortices, insula, and dorsal striatum (Volkow et al., 2008b; Verdejo-Garcia and Bechara, 2009; Koob and Volkow, 2010; Volkow et al., 2012). Especially functional imaging studies in obese human subjects suggest that the reward circuit is overactive to reward anticipation, and that inhibitory networks cannot control the reward circuit sufficiently (Kelley and Berridge, 2002; Volkow and Wise, 2005; Stoeckel et al., 2008; Volkow et al., 2008a; Stice et al., 2011; Nummenmaa et al., 2012). Also altered reward system connectivity has been proposed to play a significant role in human obesity (Gupta et al., 2015; Marques-Iturria et al., 2015). However, the role of the opioidergic 'liking' and dopaminergic 'wanting' neuroreceptor systems in human obesity remains vague.

2.2.2 *Dopaminergic system in reward functions and obesity*

Olds and Milner observed more than 60 years ago that the dopaminergic system plays an important role in reward (Olds and Milner, 1954). This has been confirmed in many subsequent studies. For instance, blockade of dopaminergic system resulted in attenuation of reward properties of food in rats (Wise et al., 1978). Dopamine receptors D₁ and D₂ are the most abundant dopamine receptor types in the human brain, and they have specific roles in the reward learning and feeding (Nakanishi et al., 2014). D₁ and D₂ receptors have own distinct signalling pathways with different downstream signalling molecules, and thus their responses to appetite control are different. Consequently, D₂ receptor stimulation causes

decrease of palatable food intake in rats, but stimulation of D₁ receptors increases it (Cooper and Al-Naser, 2006). The balance between D₁ and D₂ receptors is thus important in feeding behaviour, but the role of different subtypes still remains elusive.

Mesolimbic dopamine system is crucial in learning how natural reward such as food can be found, and it also directs animal behaviour towards the desired reward (Palmiter, 2007; Kenny, 2011). Mice unable to synthesize dopamine are hypoactive and have no motivation to eat, but feeding and moving can be restored by L-dihydroxyphenylalanine (L-DOPA) injections (Zhou and Palmiter, 1995). D₂R density correlates negatively with body weight in rats (Michaelides et al., 2012), and mice with a lower density of D₂R in the putamen exhibit more weight gain than mice with a higher density of D₂R after a high-fat diet (Huang et al., 2006). Thus, low expression of D₂R may lead to reward deficiency and increased motivation to eat.

Furthermore, rats on energy-dense cafeteria diet have decreased D₂R expression as well as depressed dopamine release in ventral striatum, and D₂R knockout mice soon develop compulsive eating habit (Geiger et al., 2009; Johnson and Kenny, 2010). Interestingly, cafeteria diet stimulates dopamine release in obese animals, whereas normal laboratory chow does not (Geiger et al., 2009). This supports the hyporeactivity theory in obesity, in which blunted dopamine release urges obese animals to eat palatable food in order to get the normal stimulus.

Human studies have also suggested the importance of mesolimbic D₂R in obesity. There are clear changes in D₂R expression and function in obese subjects (Stice et al., 2011; Salamone and Correa, 2013). PET studies also point towards the role of D₂R in obesity and feeding. A PET study using D₂R antagonist [¹¹C]raclopride with non-obese human subjects shows that food intake leads to dopamine release in dorsal striatum, and this is correlated with the experienced pleasure from the food. However, no correlation with desire to eat or satiety was observed (Small et al., 2003).

Some PET studies have also demonstrated that reduced baseline D₂R availability in striatum may contribute to overeating in humans (Wang et al., 2001; Volkow et al., 2008b; de Weijer et al., 2011). Moreover, both amphetamine (van de Giessen et al., 2014) and calorie-intake (Wang et al., 2014) triggered dopamine release is lowered among obese. However, contradicting evidence on lowered D₂R availability in obese human subjects has emerged lately (Dunn et al., 2012; Eisenstein et al., 2013; Guo et al., 2014). Overall, the impact of some of these studies is somewhat elusive, partly due to quite small sample sizes and different radioligands. In addition, new evidence links altered D₂R signalling to lowered physical activity rather than compulsive overeating (Beeler et al., 2015).

Presynaptic dopamine transporters (DAT) may play a significant role in obesity, regulating the amount of extracellular dopamine in the synaptic cleft. DAT-deficient mice have more extracellular dopamine, which leads to excessive feeding (Pecina et al., 2003). In addition, high fat diet reduces striatal DAT availability in mice (South and Huang, 2008), but lowered dopamine reuptake may occur without altering the amount of DAT protein (Cone et al., 2013). Few human studies exist, and these have yielded conflicting results. One SPECT study showed that striatal DAT availability has a negative correlation with BMI (Chen et al., 2008), while two SPECT studies with different radioligands could not find any association between BMI and DAT availability (Thomsen et al., 2013; van de Giessen et al., 2013), which makes the role of DAT in human obesity debatable.

The genetic data support the importance of the dopaminergic system in obesity. D₂ receptor variants are likely important for weight gain. Obesity and blunted striatal response to food is moderated by D₂R TaqI A1 allele (Stice et al., 2008). Carpenter and colleagues have recently showed that TaqI A1 allele was significantly associated with BMI (Carpenter et al., 2013). More recently, no association between TaqI A1 allele and adiposity was observed in a large population-based sample (Hardman et al., 2013). Thus, although contribution of dopaminergic system is presumable in human obesity, the actual mechanisms how D₂Rs affect overeating remain unresolved.

2.2.3 *Endogenous opioid system in human reward and obesity*

Animal studies have demonstrated that the endogenous opioid system is closely involved in the mammalian appetite control. It was initially found that opioid antagonist naloxone suppress appetite in rats (Holtzman, 1979). Subsequent animal studies have confirmed that MOR agonists increase and antagonists decrease liking of palatable foods and food intake (Yeomans and Gray, 2002; Bodnar, 2008; Gosnell and Levine, 2009; Pecina and Smith, 2010; Nogueiras et al., 2012). Long-lasting MOR antagonism reduces hyperphagia in rats, showing that endogenous MOR signalling in the nucleus accumbens is necessary for hedonic eating processes (Shin et al., 2010). Recent work with rats indicates that non-selective opioid antagonism decreases food intake and BMI (Ibrahim et al., 2015). Selective MOR antagonism reduces also food-seeking and binge eating in rats (Giuliano et al., 2012). While opioid antagonism reduces feeding, it also lowers dopamine release in ventral striatum (Sahr et al., 2008), proposing a close interaction between these two receptor systems.

Animal work suggests that there are apparent changes in MOR expression and function in obesity. MOR expression decreases after long-term access to palatable food, but increases after withdrawal (Pitman and Borgland, 2015). However conflicting data also exists. For instance, one study found that rats susceptible to obesity have increased expression of MOR compared to rats that are resistant to diet-induced obesity (Barnes et al., 2006). Moreover, obesity increases MOR binding assessed with autoradiography in some parts of the rat brain, which was thought to be due to decreased release of endogenous opioid peptides (Smith et al., 2002). MOR knockout mice have significantly decreased consumption of sucrose solution compared to wild type mice (Ostlund et al., 2013), while MOR deficient mice have decreased motivation to eat (Papaleo et al., 2007) and resistance to diet-induced obesity (Tabarin et al., 2005; Zuberi et al., 2008).

Genetic data also points to the contribution of MOR in obesity. The MOR gene *OPRM1* modulates the intake of fat and possibly risk for gaining weight in humans (Haghighi et al., 2013). Obese patients with binge-eating disorder have more often gain-of-function G allele in *OPRM1* but obese without binge-eating have the "loss-of-function" A1 allele in D2 receptor gene (Davis et al., 2009). However, also studies with no association with *OPRM1* and obesity exists (Hardman et al., 2013).

Human studies concentrating on endogenous system and obesity are however sparse. Bulimia nervosa (with normal BMI) has been associated with decreased MOR availability in the left insular cortex, and MOR availability is negatively correlated with recent fasting

behaviour (Bencherif et al., 2005). Another study using fMRI showed that MOR antagonism leads to significant reduction in responses to high-calorie food images among binge-eating obese subjects (Cambridge et al., 2013). It is still unclear how endogenous opioid system regulates human appetite, and what is the role of MOR system in human obesity and weight loss.

2.2.4 Interaction between dopaminergic and opioidergic systems in obesity

There is growing evidence that MORs control the release of dopamine through inhibiting GABAergic interneurons in ventral tegmental area (VTA) (Spanagel et al., 1992; Kalivas, 1993; Volkow and Wise, 2005; Rada et al., 2010; Jalabert et al., 2011; Chartoff and Connery, 2014). Furthermore, VTA dopamine neurons express MOR postsynaptically, and there seems to be direct inhibition between MOR and dopamine neurons without GABAergic signalling (Margolis and Hjelmstad, 2014). Tight interaction between dopaminergic and opioidergic systems has been proposed in human reward functions (Le Merrer et al., 2009), but only a few studies have actually investigated this. Data comes mainly from research on drugs of abuse (Volkow, 2010). Dopamine-stimulating drugs such as cocaine and amphetamine cause release of endogenous opioids (Soderman and Unterwald, 2009; Colasanti et al., 2012), which further suggests the interaction of these two systems in reward processing.

The cross-talk between opioidergic and dopaminergic system may underlie aberrant reward-related behaviour, such as excessive feeding pattern. Animal studies have indeed confirmed the interaction between these two systems in food intake. Intravenous administration of MOR agonists triggers dopamine release but also induces eating (Yeomans and Gray, 2002), and MOR antagonists block dopamine release and reduce the amount of food that rats consume (Taber et al., 1998). The interaction between MOR and D₂R receptor systems is important in regulating appetite, but the actual mechanisms are still uncertain. Data comes from preclinical studies, and practically no data on human subjects exist. The role of interaction in human obesity is completely unknown.

2.2.5 Is obesity an addictive disorder?

Because of the apparent changes in the reward circuit in obesity, parallels have been drawn between obesity and addictive disorders such as drug addiction. However, most evidence supporting this view comes from animal studies (Ziauddeen and Fletcher, 2013). As reviewed above, dopaminergic pathways – especially the mesolimbic pathway from ventral tegmental area to nucleus accumbens – regulate reward-related behaviour. Animal studies have shown that feeding increases extracellular dopamine concentration in ventral striatum (Bassareo and Di Chiara, 1997), which resembles the effect that drugs of abuse have. Both drugs of abuse and food can cause synaptic modifications in the mesolimbic dopaminergic system (DiLeone et al., 2012; Baik, 2013). Exposure to drugs of abuse,

such as cocaine or amphetamine, causes a phenomenon known as behavioural sensitization, which leads to enhanced dopamine release in ventral striatum after drug intake, but there are changes in the dopamine receptor availabilities as well (Steketee and Kalivas, 2011). These drug-induced changes may have similarities with the reactions caused by natural reward such as food.

So-called food addiction theory became popular when similar patterns of altered neurotransmission were observed in human subjects with addictive disorders and obesity. Both food and drug-related cues activate same areas of the reward circuit in fMRI studies (Wang et al., 2009; Gearhardt et al., 2011). Moreover, obese subjects and individuals with substance abuse show reduced expression of D₂R in striatal regions of the brain. Cocaine use decreases D₂R density in monkeys, and lowered levels may persist even up to one year of abstinence (Nader et al., 2006). Human studies indicate that alcohol and drug dependence lower D₂R availability in the striatum (Volkow et al., 1996; Volkow et al., 2001; Martinez et al., 2012), and PET imaging has revealed lower baseline D₂R density in the striatum both in addictive disorders and obesity (Wang et al., 2001). In this study, D₂R density was shown to be proportional to BMI. This was taken to suggest that lowered D₂R density would make individuals prone to overeating because of food-induced reward deficiency. Other PET studies in morbidly obese human subjects have also showed lower striatal D₂R availability (Volkow et al., 2008b; de Weijer et al., 2011), but there are also many conflicting studies showing unaltered availability in the striatum (Haltia et al., 2007b; Haltia et al., 2008; Steele et al., 2010; Eisenstein et al., 2013; Guo et al., 2014).

The role of opioid system in addictive disorders is less well understood. Animal studies show that persistent MOR upregulation occurs in rats both during the use of cocaine and after withdrawal. This may be due to chronic reduction in endogenous opioid release (Bailey et al., 2005). Similarly, cocaine dependence in human subjects is linked to increased MOR availability in large areas, including anterior cingulate and frontal cortex (Gorelick et al., 2005). Alcohol dependence is associated with higher MOR availability in ventral striatum (Heinz et al., 2005; Weerts et al., 2011). On the other hand, opioid addiction may lead to decreased MOR availability, which may subsequently lead to opioid tolerance (Koch and Holtt, 2008). However, the effects of opioids to MOR protein levels are diverse and possibly substance specific (Le Merrer et al., 2009; Whistler, 2012).

Altogether, drug addictions seem to be a neurochemically and behaviourally different state compared with obesity. In contrast to eating, drug addictions are not affected by natural homeostatic mechanisms. Even from a pharmacological point of view, withdrawal symptoms for obesity and drug addiction are different. Moreover, food-related environmental factors begin to affect us already at perinatal stage (Carnell et al., 2012; Grissom et al., 2014). It is thus possible that the basic processes that direct one's motivation towards certain goal – may it be drug or food – can be quite similar, although neurobiologically complex (Salamone and Correa, 2013). However, other processes that maintain the pathological eating habits seem to be different than those supporting drug addiction. Obesity is also a very heterogeneous disorder, and a simple model such as food addiction would just appear as a hindrance to future obesity research (Ziauddeen et al., 2012).

2.3 Obesity and brain atrophy

Obesity can cause severe damage to internal organs, for example heart, skeletal muscle, and liver (Unger, 2003). In addition, obesity has been associated with many co-morbidities such as hypertension (Brown et al., 2000), coronary disease (Jousilahti et al., 1996), and type 2 diabetes (Kopelman, 2000). Obesity causes adverse effects to central nervous system based on animal studies (Mattson et al., 2002), but obesity is a notable risk factor to neurodegenerative disorders such as the Alzheimer's disease in humans (Gustafson et al., 2003; Jagust et al., 2005; Kivipelto et al., 2005).

Hypertension and diabetes are associated with decreased brain volume and damage (Raz et al., 2003; Taki et al., 2004; Korf et al., 2007; Gons et al., 2010; Yau et al., 2010; Debette et al., 2011; Hsu et al., 2012; Climie et al., 2015), but also obesity decreases global brain volume (Ward et al., 2005). Several studies using voxel-based morphometry (VBM) approach have demonstrated that obese people have global and focal decreases in brain grey matter (GM) density (Taki et al., 2008; Walther et al., 2010; Horstmann et al., 2011; Brooks et al., 2013; Bobb et al., 2014; Lou et al., 2014; Janowitz et al., 2015). Moreover, lower GM densities in obese subjects have been observed in many focal areas (Pannacciulli et al., 2006; Raji et al., 2010). Frontal and limbic areas seem to be affected already in obese children and adolescents (Alosco et al., 2014a).

It is not clear how weight gain affects the brain, and many physiological processes might be involved. Increased adipose tissue causes a chronic, low-grade inflammation, which is initiated by excess of nutrients in metabolic cells (Gregor and Hotamisligil, 2011; Lumeng and Saltiel, 2011), and which in turn decreases brain GM density (Debette et al., 2010; Cazettes et al., 2011). A high level of C-reactive protein is linked to brain alterations and impaired cognitive functions among obese subjects (van Dijk et al., 2005; Sweat et al., 2008). Also adipokines such as leptin can affect brain structure, leading to decreased local and focal GM density (Pannacciulli et al., 2007; Gunstad et al., 2008; Mueller et al., 2014). Chronic metabolic inflammation may indeed be the key factor behind observed brain density alterations.

Obesity also causes atrophy in brain's white matter (WM). Atrophy in the basal ganglia and corona radiata has been observed among obese subjects (Raji et al., 2010), although one conflicting study has reported increased WM density in obesity (Haltia et al., 2007a). Two tensor-based morphometry studies have observed reductions in both GM and WM densities in obese subjects (Ho et al., 2010; Cole et al., 2013). There is also growing evidence that obesity has a negative effect on the structural integrity of WM, as measured with Diffusion Tensor Imaging (DTI) (Cazettes et al., 2011; Marks et al., 2011; Stanek et al., 2011; Verstynen et al., 2012; Xu et al., 2013; Lou et al., 2014; Mueller et al., 2014; Marques-Iturria et al., 2015; Kullmann et al., 2016). Some of these alterations may be sex-dependent (Mueller et al., 2011). Hypothalamic damage measured with DTI has been linked to poor cognitive performance in obese subjects (Puig et al., 2015). Factors behind WM changes are probably the same than with GM changes. Low-grade inflammation is an important factor behind WM alteration (Puig et al., 2015), while type 2 diabetes (Yau et al., 2009; Yau et al., 2010) and hypertension (Maclulich et al., 2009; Gons et al., 2010) are associated with damage to WM tracts. Abnormal cholesterol profile can also have a negative effect on WM integrity in obesity (Cohen et al., 2011). Among children and

adolescents, obesity has no clear effect on WM integrity (Alosco et al., 2014a). It is possible that changes to WM appear later on life, and GM is more susceptible to damage even at the earlier stages of life.

It is still elusive whether aforementioned changes in brain precede or follow weight gain. Few prospective studies exist. Yokum and colleagues observed reduced brain GM and WM densities in the obese subjects, and at one-year follow-up they found that low GM density in the areas implicated especially in inhibitory functions are associated with future weight gain. Furthermore, reductions in WM density seem to be secondary to weight gain (Yokum et al., 2012). In a recent 5-year follow-up study, higher baseline BMI was associated with greater decline in temporal and occipital GM density (Bobb et al., 2014). Although it seems likely that metabolic factors negatively affect brain structure, it is possible that some of the observed alterations especially in the brain areas associated with reward and behavioural control have preceded obesity and led to pathological eating behaviour (Pannacciulli et al., 2006; Yokum et al., 2012).

2.4 Does weight loss alter brain function and structure?

Many weight loss strategies have been developed to tackle the obesity epidemic. Behavioural interventions include cognitive therapies, dietary modifications, and increased exercise, which all focus on supporting more favourable energy balance. Unfortunately, these therapies have not been very successful. A meta-analysis on behavioural interventions resulted only in mean weight loss from 5 to 9 % at six months, after which regain of weight was observed in many subjects (Franz et al., 2007).

Bariatric surgery is the most effective method for weight loss in obesity (Gloy et al., 2013; Maggard-Gibbons et al., 2013). Bariatric surgery procedures are much more effective than intensive medical therapy to reach weight loss and glycaemic control (Schauer et al., 2014). Systematic reviews show that bariatric surgery leads to substantial weight loss and remission of diabetes (Buchwald et al., 2009), but it also prevents from future type 2 diabetes (Carlsson et al., 2012) and cardiovascular deaths (Sjostrom et al., 2012). Surgery also affects the appetite. For instance, studies with fMRI have shown reduced neural responsivity as well as desire for eating and liking of high-calorie foods after bariatric surgery (Ochner et al., 2012; Frank et al., 2014). One fMRI study showed small differences in reactions to visual food cues between subjects who underwent surgical versus behavioural weight loss (Bruce et al., 2014).

The actual molecular mechanisms of how bariatric surgery affects the appetite control in the brain are still unknown. Gut hormones are affected by bariatric surgery. Elevated PYY levels and decreased ghrelin levels are observed among the subjects who underwent a bariatric surgery (Karamanakos et al., 2008; Munzberg et al., 2015). Moreover, significant improvement of GLP-1 response to food intake has also been observed (Morinigo et al., 2006). Moreover, enteroendocrine melanocortin pathway may have importance in the postsurgical suppression of appetite (Manning et al., 2015), but also psychological factors such as aversive conditioning (arising from the fear of unpleasant feelings like dumping after the surgery) may be involved (Shin and Berthoud, 2011). Bariatric surgery and following weight loss also improves the glucose metabolism in the brain (Tuulari et al.,

2013), which may partly affect the control of appetite. Recent animal work suggests that both bariatric surgery and caloric restriction increase the amount of dopamine but decrease the amount of noradrenaline in dorsal striatum compared to fed animals (Reddy et al., 2014).

Cross-sectional studies do not reveal whether the changes in neuroreceptor systems and brain densities have existed before weight gain or have developed after weight gain. Bariatric surgery provides a method for investigating whether molecular and structural changes in the brain are causes or consequences of obesity. Two small-scale human PET studies have investigated the effects of bariatric surgery and following weight loss to D₂Rs. Steele and colleagues observed increased availability after the binding after the bariatric surgery (Steele et al., 2010). On the other hand, Dunn and colleagues measured decreased D₂R availability in many parts of the reward circuit (Dunn et al., 2010). Moreover, one SPECT study with 19 female obese subjects observed no change in striatal D₂R availability 6 weeks after RYGB surgery (de Weijer et al., 2014). It remains completely unknown how weight loss influences the MOR availability. It is also previously unsolved how receptor availabilities affect mental states and behaviour in obesity, assessed by different questionnaires measuring reward functioning and eating behaviour. Moreover, there are no studies addressing the changes in brain GM or WM densities after weight loss.

2.5 Summary of the literature

Altogether, existing evidence suggests that obesity affects both brain structure and function of specific neurotransmitter systems. To date, reductions in global and focal GM densities have been shown in many studies, but research concentrating to WM integrity and obesity is still fractional. The actual mechanisms causing GM and WM density alterations remain unresolved. Furthermore, molecular function of reward circuit and its interplay with homeostatic mechanisms of food intake in obesity is not fully understood. Critically, the role of endogenous opioid system in human obesity remains elusive, albeit animal research support its contribution to human obesity as well. Finally, only a few longitudinal studies examining the brain structure and function over time exists. The link between obesity and brain-level changes remains thus unclear.

3 OBJECTIVES OF THE STUDY

This doctoral thesis presents a multimodal neuroimaging approach on the neural basis of human obesity using positron emission tomography (PET) and magnetic resonance imaging (MRI), including both voxel-based morphometry (VBM) and diffusion tensor imaging (DTI). Brain neurotransmitter systems and anatomy was investigated both in morbidly obese and non-obese subjects using aforementioned brain imaging methods. Obese subjects underwent bariatric surgery during the project. They were scanned before and six months after the operation. Thus, it was possible to evaluate whether possible alterations in obese subjects' brains change after the surgical operation and concomitant weight loss, or whether the alterations represent stable individual characteristics.

The specific objectives of this thesis are:

1. To characterize the differences in two specific neurotransmitter systems (MOR and D₂R) between obese and non-obese subjects (**Study I**).
2. To assess the role of interactions between MOR and D₂R in obesity (**Study II**).
3. To investigate the effect of bariatric surgery and following weight loss to MOR and D₂R (**Study III**).
4. To characterize the differences in brain white and gray matter densities as well as white matter integrity between obese and non-obese subjects (**Study IV**).
5. To determine the effect of bariatric surgery and following weight loss brain white and gray matter densities in obesity (**Study V**).

4 GENERAL METHODOLOGY

4.1 Subjects

Subjects were collected from two larger studies, Sleevepass (NCT00793143) and SleevePET2 (NCT01373892) (<http://www.clinicaltrials.gov>), both of which investigated the effects of bariatric surgery to various organ systems including the brain (Table 1). Altogether, 49 morbidly obese subjects and 42 non-obese control subjects participated in this project.

Morbidly obese study subjects were recruited from a patient population selected to undergo bariatric surgery as their standard clinical treatment for morbid obesity. Non-obese control subjects were volunteers recruited using newspaper advertisements. Morbidly obese subjects and controls were matched for age, height, and sex.

Studies were conducted in accordance with the Declaration of Helsinki. Study protocol, patient information, and informed consent form were submitted to the Ethical Committee of the Hospital District of the South-Western Finland and the permission was granted before the recruitment of the subjects. All the subjects signed the ethical committee approved informed consent form prior to studies.

Table 1. Number of participants in each study. Participants were all female unless otherwise stated.

	Sleevepass (NCT00793143)	SleevePET2 (NCT01373892)
Study I		13 morbidly obese 14 controls
Study II		25 morbidly obese 20 controls
Study III		16 morbidly obese 14 controls
Study IV	23 morbidly obese (5 males) 22 controls (7 males)	
Study V	24 morbidly obese (5 males) 15 controls (6 males)	23 morbidly obese 14 controls

For the morbidly obese subjects, inclusion criteria were 1) BMI ≥ 40 kg/m², or BMI ≥ 35 kg/m² if there was an additional risk factor such as type 2 diabetes or hypertension, and 2) age 18-60 years. Exclusion criteria were 1) diabetes requiring insulin treatment, 2) BMI over 60 kg/m² or weight over 170 kg, and 3) eating disorders or severe mental disorders.

For the control subjects, inclusion criteria were 1) BMI 18-27 kg/m², 2) age 18-60 years 3), and normal oral glucose tolerance test (OGTT), and exclusion criteria were 1) regular use of any medication, and 2) any chronic disease.

For both groups, exclusion criteria included 1) excessive use of alcohol or any use of other drug of abuse, 2) poor compliance, 3) pregnancy, 4) past dose of radiation from nuclear imaging studies, 5) presence of any ferromagnetic objects that would contraindicate MR imaging, and 6) notable claustrophobia that would possibly contraindicate brain imaging studies.

4.2 Overall study design

The main research site of this project was Turku PET Centre (<http://www.turkupetcentre.fi>). Clinical screening consisted of medical history, physical examination, anthropometric measurements as well as laboratory tests including an OGTT. Depression was assessed using Beck Depression Inventory II (BDI-II) questionnaire (Beck et al., 1996), anxiety levels were measured using State-Trait Anxiety Inventory (STAI) questionnaire (Spielberger et al., 1983), food craving and eating behaviour were assessed with Food Craving Questionnaire (FCQ) (Cepeda-Benito et al., 2000), Dutch Eating Behaviour Questionnaire (DEBQ) (van Strien et al., 1996), and Yale Food Addiction Scale (YFAS) (Gearhardt et al., 2009).

After the clinical screening, baseline MRI and PET imaging studies were performed. These studies were performed before the standard very low calorie diet, after which the morbidly obese proceeded to bariatric surgery. Non-obese controls were studied only once. For the morbidly obese subjects, imaging procedures were repeated 6 months after the bariatric surgery (Figure 1). They were also clinically examined both pre- and post-operatively.

Morbidly obese subjects:



Non-obese control subjects:

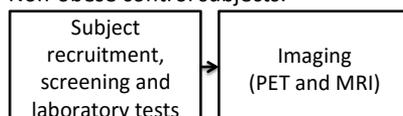


Figure 1. Overall design of the studies.

4.3 Positron Emission Tomography (PET)

Positron emission tomography (PET) is a quantitative and non-invasive *in vivo* imaging method, which utilizes positron-emitting isotopes to study various physiologic, metabolic, and functional processes in the human body. A wide variety of biological molecules can be labelled with radioactive isotopes (most commonly ^{11}C , ^{18}F , and ^{15}O). The labelled molecules are called radioligands, which can be used to investigate, for example, glucose metabolism and receptor-ligand interactions. Almost every biological system can be imaged with PET as long as molecules binding specifically to the target system can be labelled with radioactive isotopes.

A cyclotron is used to produce the unstable isotopes that have one excess proton in their nucleus. When a radioligand injected in the human body, the unstable nucleus undergoes positron decay, causing the nucleus to emit a positron (e^+) and a neutrino (ν) (Turkington, 2001). The positron can travel only a short distance in the tissue after which a collision with an electron will occur. This collision is called annihilation, in which the positron and the electron will be transformed into two 511 keV photons travelling to opposite directions (Figure 2). (Turkington, 2001; Bailey, 2005).

The detectors in the PET scanner identify these two photons. This simultaneous detection is called a coincidence event, which is detected by the scanner (Figure 2). Because the photons are thought to travel to opposite directions, an imaginary line known as line of response (LOR) can be drawn between the detectors. Each LOR is registered by its location and the angle of orientation, and coincidence events are often histogrammed according to the LORs in a table called sinogram. Finally, the data in sinograms are reconstructed into PET images. These PET images are degraded by many physical factors, such as scatter (false localization of the event due to aberration from the original LOR), attenuation (reduced signal due to photon absorption by tissue), random events (simultaneous false counts interpreted as true counts by the scanner), and dead-time (inability to record true counts at high event rates), but at least some of these can be corrected by specific techniques. (Turkington, 2001; Bailey, 2005).

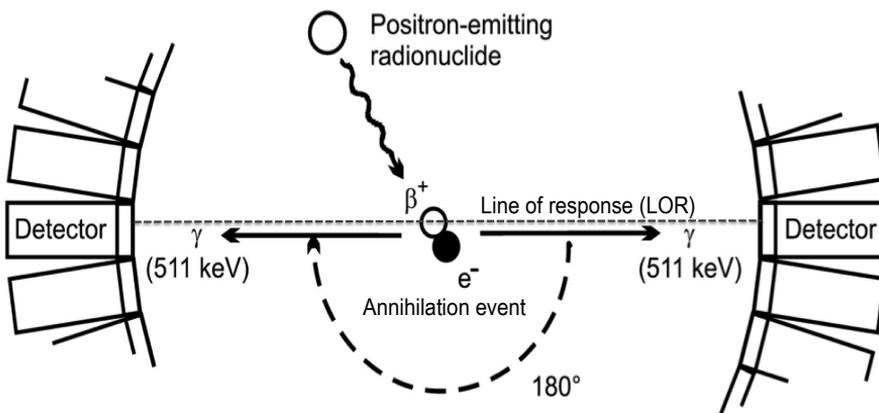


Figure 2. A schematic illustration of annihilation. Modified from (Verel et al., 2005).

4.3.1 PET image acquisition (Studies I-III)

In the PET imaging studies of this project, two different neurotransmitter systems were focused on (Figure 3). Dopaminergic system was studied with [^{11}C]raclopride, which is a dopamine D₂ receptor antagonist binding mainly to striatal and thalamic areas (Farde et al., 1986). Opioidergic system was measured with [^{11}C]carfentanil, which is a high-affinity agonist to μ -opioid receptors (Frost et al., 1985). These radioligands are well validated for human studies, having high test-retest reliability (Hirvonen et al., 2003; Hirvonen et al., 2009). In addition, these radioligands have been used in numerous clinical settings during the past years.

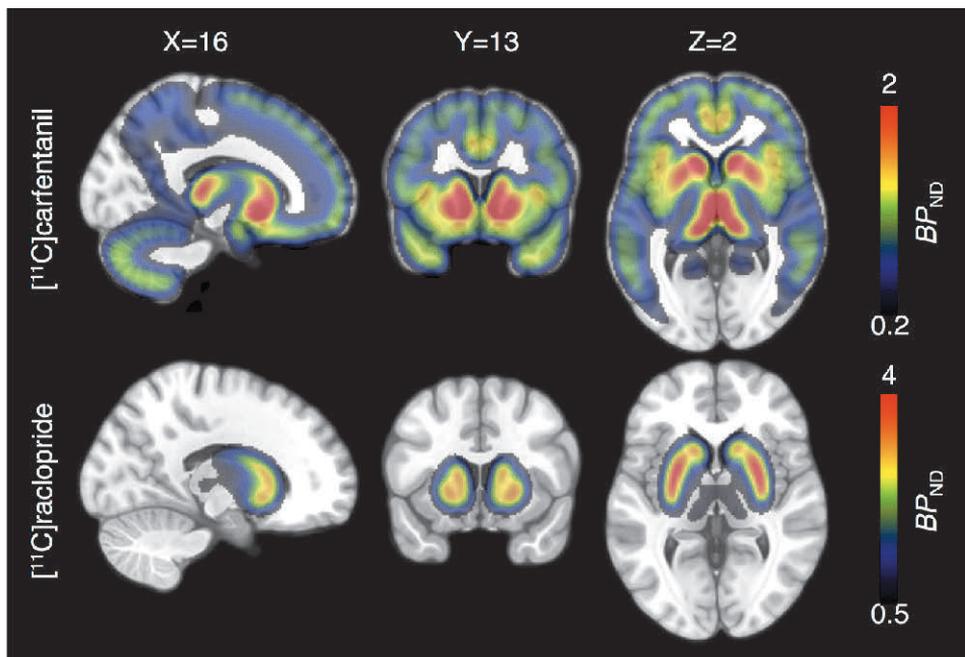


Figure 3. Distribution of μ -opioid receptors measured with [^{11}C]carfentanil (as indexed by BP_{ND} levels; upper panel) and dopamine D₂ receptors measured with [^{11}C]raclopride (lower panel) in the human brain (Original publication II).

Synthesis of the both radioligands took place in the Accelerator Laboratory of Turku PET Centre at Åbo Akademi University. CC18/9 cyclotron (Efremov Institute, Saint-Petersburg, Russia) was used to produce [^{11}C]methane, which was later on converted into [^{11}C]methyl triflate and linked to precursor molecules. The identity, radiochemical purity and the specific radioactivity of the products were determined using high performance liquid chromatography and UV detection. Both radioligands had high radiochemical purity (>99 percent). For detailed information of the radioligand production, see the original publication (Karlsson et al., 2015).

Subjects were scanned during satiated state. Before the PET scans, CT scans were taken to obtain attenuation maps and reference anatomical images of the brain. Radioligand was administered intravenously as bolus injections via a catheter placed in the antecubital vein. Radioactivity in brain was measured with the GE Healthcare Discovery™ 690 PET/CT scanner (General Electric Medical Systems, Milwaukee, WI, USA; Figure 4). Effective resolution of the PET scanner was 4.7 mm full width at half maximum (FWHM). Total scanning time was 51 minutes during which 13 time frames were collected (3 x 1 min, 4 x 3 min, 6 x 6 min). Data were corrected for dead-time, decay, and CT-measured photon attenuation. Brain scans covered the whole brain in 3D mode, and dynamic PET-scans were reconstructed using time-of-flight information.

To exclude structural abnormalities and to provide anatomical reference images for the PET scans, MR imaging was performed with Philips Gyroscan Intera 1.5 T CV Nova Dual scanner (Philips Medical Systems, Best, Netherlands). Whole-brain T1-weighted images were obtained using Repetition time (TR) = 25 ms, Echo time (TE) = 4.6 ms, flip angle = 30°, scan time = 376 s, voxel size = 1 mm³.

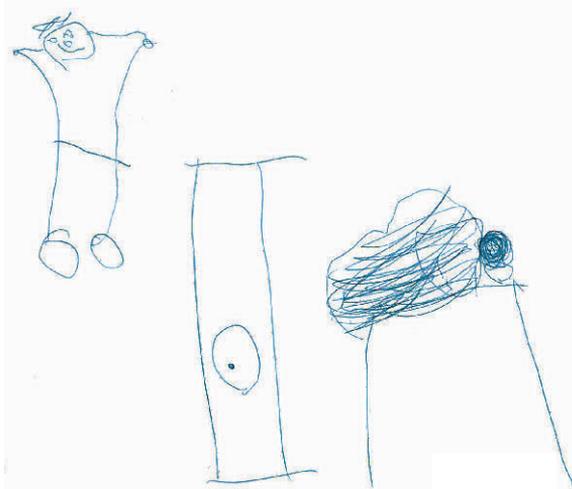


Figure 4. Schematic illustration of GE Healthcare Discovery™ 690 PET/CT scanner located at Turku PET Centre (drawing by 3-year-old Kerttu Ranki)

4.3.2 PET data analysis (Studies I-III)

Reconstructed PET images need to be modelled in order to convert radioactivity concentration into meaningful biological data, such as receptor binding in the brain. Kinetic compartmental models are used to estimate the radiotracer pharmacokinetics (Gunn et al., 1997). Models also provide assumptions about rate constants between the distinct compartments. In all the PET studies to be included in this thesis, a two-tissue

compartment model known as the simplified reference tissue model (SRTM) was utilized (Figure 5). It is based on the comparison of radioligand concentration in receptor-rich to receptor-free regions. Unlike in dynamic PET studies, where arterial plasma concentration of the radiotracer is needed as input data, SRTM allows quantification of receptor availability without any arterial cannulation or blood samples (Lammertsma and Hume, 1996). In this model, time activity curves (TAC) from specific reference regions serve as input data (Gunn et al., 1997).

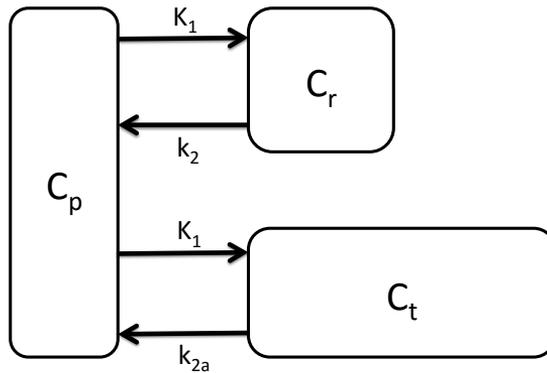


Figure 5. Schematic illustration of the simplified reference tissue model. Adopted from (Lammertsma and Hume, 1996; Lammertsma, 2014). C_p = tracer concentration in arterial plasma; C_r = tracer concentration in the reference tissue; C_t = tracer concentration in the target region; K_1 = rate constant for transfer from arterial plasma to tissue; k_2 = rate constant for transfer from tissue to arterial plasma; k_{2a} = apparent rate constant for transfer from tissue to plasma.

Using SRTM, receptor availability can be measured for each voxel as the binding potential (BP_{ND}), which is the ratio of specific to non-displaceable binding in brain (Innis et al., 2007). In this model BP_{ND} is calculated using the following equation:

$$BP_{ND} = f_{ND} \times 1/K_d \times B_{max}$$

In the equation, f_{ND} stands for the free fraction of the ligand in the non-displaceable tissue, $1/K_d$ is the receptor affinity and B_{max} is the receptor availability. Consequently, BP_{ND} is the product of all these three factors. SRTM rests on numerous assumptions. First, a reference tissue is assumed to have fully non-specific binding. Second, non-specific binding is assumed to be same in both reference and target regions. Third, free ligand and non-specifically bound ligand cannot be separated, and the model assumes that the exchange between these compartments has to be fast to be considered as one compartment.

Before statistical analysis, head motion during scanning as well as individual differences

in brain anatomy need to be accounted for. In the present PET studies, Statistical parametric mapping 8 (SPM8) software (Wellcome Trust Centre for Neuroimaging, London, UK; www.fil.ion.ucl.ac.uk/spm/), running on Matlab R2012a (The Mathworks Inc., Sherborn, Massachusetts), was used in the preprocessing of the PET images. First, head motion was corrected by realigning the dynamic PET images frame-to-frame. Second, subjects' T1-weighted MR images were coregistered to the summation images calculated from previously realigned frames. PMOD 3.4 software (PMOD Technologies Ltd., Zurich, Switzerland) was used to manually draw the reference regions. Occipital cortex was delineated as the reference region for [¹¹C]carfentanil and cerebellum for [¹¹C]raclopride. TACs needed for SRTM were acquired from the reference regions using PMOD software. Normalization of the parametric BP_{ND} images into MNI space was done by first coregistering the PET images with T1-weighted MR images. After normalization of the T1-weighted images, the obtained warping parameters were applied to the PET images. Normalized parametric BP_{ND} maps were smoothed with a Gaussian kernel of 8 mm FWHM.

In the full-volume statistical analyses, voxel-wise differences in [¹¹C]carfentanil and [¹¹C]raclopride BP_{ND} s were compared using independent samples t-tests between morbidly obese and non-obese groups (Studies I and II) and repeated measures t-test within subjects (Study III) in SPM8. The statistical threshold was set at $p < 0.05$, with the False Discovery Rate (FDR) corrected at cluster level. In addition to the full-volume SPM analyses, the AAL (Tzourio-Mazoyer et al., 2002) and Anatomy (Eickhoff et al., 2005) toolboxes were used to automatically delineate ROIs and extract ROI-wise BP_{ND} s in different brain areas: ventral striatum, dorsal caudate nucleus, putamen, insula, amygdala, thalamus, orbitofrontal cortex, anterior cingulate cortex, medial cingulate cortex, and posterior cingulate cortex.

In all the PET studies, the same amount of radioactivity was injected to both obese and non-obese subjects. Although this may lead to smaller count rates in obese subjects' brains, it is unlikely that reconstruction used by GE Healthcare DiscoveryTM 690 PET/CT scanner would cause an underestimation of SRTM derived BP_{ND} . To further ensure that BP_{ND} s were accurate, the injected amounts of radioactivity per weight (kg) were correlated with MOR and D₂R availabilities in all ROIs, but no correlation was found.

Associations between ROI-wise BP_{ND} s, questionnaire scores, and biological variables were calculated using Pearson's correlations (Studies I and III). Pearson's correlations were also used to estimate regional interactions between receptor systems (Study II). Between-groups differences in the ROI-wise Pearson correlations between receptor systems were calculated using Fisher's test (Study II).

4.4 Magnetic Resonance Imaging (MRI)

Magnetic resonance imaging (MRI) provides an outstanding non-invasive imaging method for different anatomical structures. It is based on the strong (typically > 1.5 Tesla) static magnetic field by the MRI scanner, which can be used to produce different magnetic resonance (MR) signals in order to form high-contrast images of the human body. MR signal originates from the hydrogen atoms (H^1), which are abundant in the human tissue in free water or fat molecules. Hydrogen nuclei consist of a single proton. Protons have

an intrinsic feature called the nuclear spin, which makes every proton to form a tiny magnetic field known as magnetic momentum. Without any external magnetic field (B_0), these magnetic moments are randomly oriented. However, the strong static magnetic field produced by the MRI scanner forces the magnetic moments to align in a direction of parallel or anti-parallel compared to B_0 . This results in a net magnetic field or net magnetisation (M_0). (Hendee and Morgan, 1984; Duerk, 1999; Nitz, 1999; McRobbie et al., 2006; Ridgway, 2010).

To create MR signal from M_0 , another magnetic field (B_1) is applied using scanner's transmitter / receiver coils. This field is perpendicular to B_0 , causing a rotating movement to the net magnetisation. When the duration and the amplitude of B_1 are changed, different radio frequency pulses can be generated. Radio frequency pulses cause the net magnetic moment of the nuclei, to tilt away from equilibrium, bringing them into a higher energy state. When these excitation pulses stop, spin population starts to return back to its previous alignment. This process is called relaxation. The relaxation time differs depending on the proton density and the molecular structure of the tissue. Tissue contrast in MR images arises from the differences in relaxation times between different tissues. There are two different relaxation processes utilized in MRI. The longitudinal relaxation or T1 (spin-lattice) relaxation means the longitudinal realignment of the magnetisation with B_0 , whereas transverse relaxation or T2 (spin-spin) is the process in which protons phase or dephase with each other. T1-weighted images offer excellent discrimination between water and fat, and thus differentiation of brain gray and white matter is possible. Weighting transverse (T2) on the contrary produces images in which the signals of water and fat are opposite than in T1-weighted images. (Hendee and Morgan, 1984; Duerk, 1999; McRobbie et al., 2006)

4.4.1 MR Image acquisition (Studies I-V)

MRI was performed using Philips Gyroscan Intera 1.5 T CV Nova Dual scanner. Anatomical images with 1 mm^3 resolution were acquired using a T1-weighted sequence (TR 25 ms, TE 4.6 ms, flip angle 30° , scan time 376 s). T1-weighted images were used in VBM analysis as well as reference images for PET scans. For DTI analysis, 32 non-collinear directions of gradients and non-diffusion weighted b_0 image were acquired to obtain the whole diffusion tensor, using an echo-planar imaging (EPI) single-shot sequence (TR 5947 ms, TE 89 ms, 90° flip angle, FOV $240\ 112 \times 112$ imaging matrix [reconstructed to 256×256], 3 mm slice thickness, 1 mm gap between slices, 36 transverse slices).

The volume of abdominal subcutaneous (SAT) and visceral (VAT) adipose tissue was measured for all the studies (I-V). To this end, axial T1-weighted dual fast field echo images covering the abdominal area were acquired (TR 120 ms, TE 2.3 and 4.6 ms, slice thickness 10 mm without gap). SAT and VAT were assessed from top of liver until the top of femoral bone and analysed using the SliceOmatic software version 4.3 (<http://www.tomovision.com/products/sliceomatic.htm>).

4.4.2 VBM data analysis (Studies IV-V)

Voxel-based morphometry (VBM) is a method for assessing focal brain structure differences. It allows voxel-wise comparison of brain GM and WM tissue densities between different subjects using information from T1-weighted MR images. (Ashburner and Friston, 2000). For example, comparison between a healthy control group and a group of patients with a particular condition or disease can be made. T1 images are first automatically segmented into probabilistic GM and WM volumes. Following normalization into standard stereotactic space, the smoothed GM and WM images can be compared between groups.

VBM was performed with SPM5 (Study IV) and with SPM8 (Study V) (Wellcome Trust Centre for Neuroimaging, London, UK; www.fil.ion.ucl.ac.uk/spm/). Using SPM software, spatial normalization, tissue classification, and radio-frequency bias correction were combined into a single step with segmentation to grey (GM) and white matter (WM) and cerebro-spinal fluid. Cut-off of spatial normalization was 25 mm, medium affine regularization (0.01) was used. Smoothing with a Gaussian kernel of 10 mm FWHM was performed to the segmented, normalized, and modulated GM and WM images.

General linear model (GLM) (Friston et al., 1994) was used to compare GM and WM densities between obese and non-obese groups (Study IV and V) and within subjects to assess GM and WM changes following bariatric surgery (Study V). Effects of age and gender on brain volume were controlled by modelling them as regressors of no interest. Statistical threshold was set at $p < .05$, FDR corrected at the cluster level while controlling for non-stationarity in VBM analysis (Hayasaka et al., 2004). Moreover, clusterwise GM and WM volumes were extracted using Marsbar software (<http://marsbar.sourceforge.net>) and correlated with anthropometric and metabolic variables before (Studies IV and V) and after the bariatric surgery (Study V).

4.4.3 DTI data analysis (Study IV)

Diffusion-weighted (DW) MRI is based on detecting the motion of water in different dimensions, making it suitable to image biological tissues with restricted diffusion (Le Bihan et al., 1986). Using DTI, it is possible to extract different measures of water diffusion from DW images to investigate neural microstructure. In the human brain, diffusion is quite restricted in the white matter, where myelinated axons allow the motion of water mainly along the axis of the axons. Most widely used scalars are fractional anisotropy (FA) and mean diffusivity (MD). FA shows the directionality (FA of 0 indicates free water motion to all directions i.e. isotropic diffusion, but FA of 1 refers to restricted movement to only one direction) (Basser and Pierpaoli, 1996; Alexander et al., 2007). FA is sensitive to microstructural changes, but it cannot differentiate between the types of damage. Therefore other scalars are needed. For example, MD shows the mean squared displacement of water molecules, and it cannot tell anything about the direction of the diffusion. High MD values however reflect less restricted diffusion. MD is basically the inverse measure of the membrane density and fluid viscosity, and can reveal oedema or necrosis (Alexander et al., 2011).

In the first part of the DTI analysis, DW images were corrected for eddy currents and head motion. Subsequently, fractional anisotropy (FA) and mean diffusivity (MD) diffusion tensors were computed using FDT analysis package in FSL software (www.fmrib.ox.ac.uk/fsl). MD and FA images were normalized to the MNI space using linear and nonlinear transformations and smoothing using a Gaussian kernel of 10 mm FWHM. Next, smoothed FA and MD maps were analysed using SPM5. Comparisons between obese and non-obese groups were calculated using GLM. Effects of age and gender on diffusion tensors were set as regressors of no interest. Statistical threshold was set at $T > 3.30$ and $p < .05$, FWE corrected at the cluster level.

5 RESULTS

5.1 Obesity is associated with decreased cerebral MOR availability (Study I)

The differences in MOR and D₂R availabilities between morbidly obese and non-obese subjects were characterized in a cross-sectional design. MOR and D₂R availabilities were measured with PET using [¹¹C]carfentanil and [¹¹C]raclopride, respectively. Significantly lower [¹¹C]carfentanil BP_{ND} ($p < 0.05$, FDR corrected) was found globally in the obese group compared with the non-obese group. These areas include many parts of the brain that are relevant for reward processing, such as ventral striatum, thalamus, and insula (Figure 6). BMI also correlated negatively with [¹¹C]carfentanil BP_{ND} in most of these areas. Neither full-volume SPM analysis nor ROI analysis revealed any significant differences in [¹¹C]raclopride BP_{ND} in any brain region.

MOR availability and anxiety (STAI) scores were negatively correlated in anterior cingulate cortex, medial cingulate cortex, and posterior cingulate cortex ($r_s < -0.38$, $p_s < 0.05$). Moreover, DEBQ restrained eating score negatively associated with MOR availability in ventral striatum, amygdala, and thalamus ($r_s < -0.38$, $p_s < 0.05$).

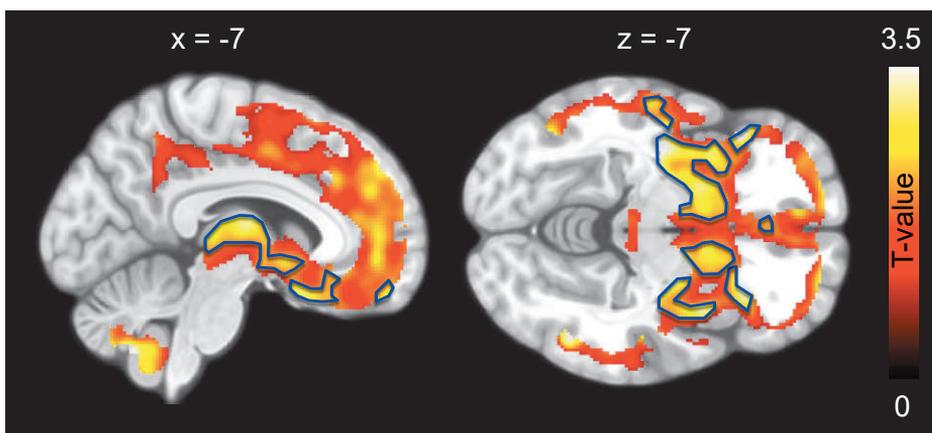


Figure 6. Brain regions where [¹¹C]carfentanil BP_{ND} is lowered in morbidly obese subjects versus non-obese subjects ($p < 0.05$, FDR corrected). The blue outline shows regions where the effect is observed with more stringent statistical threshold ($p < 0.01$, FDR corrected) (Original publication I).

5.2 Interaction between dopamine and opioid systems is disrupted in morbid obesity (Study II)

The interaction between MOR and D₂R systems was investigated in morbidly obese and non-obese subjects. MOR and D₂R availabilities were measured with PET using [¹¹C]carfentanil and [¹¹C]raclopride, respectively. Subsequently, voxel-by-voxel correlations were computed between [¹¹C]carfentanil and [¹¹C]raclopride BP_{NDS} in the obese and lean subjects.

Both voxel-level analysis and ROI analysis¹ showed that in the non-obese subjects, regional MOR and D₂R availability were positively correlated in ventral striatum and dorsal caudate, but not in putamen (Figure 7). In the morbidly obese subjects, the significant association between MOR and D₂R availability was found in dorsal caudate, but the association was disrupted in ventral striatum (Fisher's $z = 1.872$, one-tailed $p = .031$; Figure 8). The association was not driven by group differences in GM density.



Figure 7. In non-obese subjects MOR and D₂R availability were associated in ventral striatum and dorsal caudate. Colorbar shows the voxelwise Pearson correlation coefficient (Original publication II).

¹ Because [¹¹C]raclopride binding outside the striatal areas is relatively unspecific, the analysis was restricted to this region.

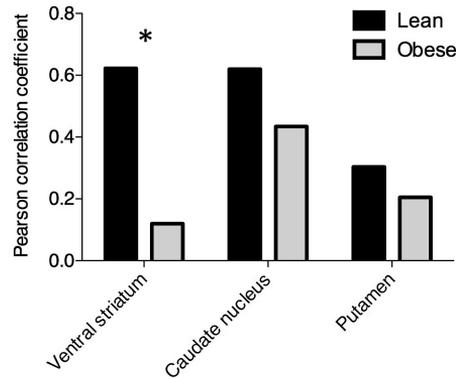


Figure 8. Association between MOR and D₂R availability was significantly decreased in ventral striatum among obese subjects ($p = .031$), but not in caudate nucleus or putamen (Original publication II).

5.3 Bariatric surgery and weight loss normalizes MOR availability in morbid obesity (Study III)

The effect of bariatric surgery induced weight loss on MOR and D₂R availability was assessed in this study. MOR and D₂R availabilities were measured in the morbidly obese subjects before and six months after the bariatric surgery using PET with [¹¹C]carfentanil and [¹¹C]raclopride. Control subjects were scanned once. Preoperatively, obese had significantly lower MOR availability globally but there were no differences in D₂R availability. Bariatric surgery resulted in mean weight loss of 26 kg. Significant increase in MOR availability was observed in many brain regions relevant for reward functions, such as ventral striatum, thalamus, amygdala, and insula ($p < 0.05$, FDR corrected; Figure 9). This effect was observed in all but one subject (15 out of 16). However, bariatric surgery and weight loss did not cause any changes in D₂R availability (Figure 9).

Before the operation, BMI correlated negatively with [¹¹C]carfentanil BP_{ND} in every ROI except for anterior cingulate cortex ($r_s < -0.36$, $p_s < 0.05$), and after the surgery, [¹¹C]carfentanil BP_{ND} was found to negatively correlate with BMI in ventral striatum and dorsal caudate ($r_s < -0.45$, $p_s < 0.05$). Glycaemic status or insulin sensitivity did not affect MOR availability before or after the operation.

Questionnaire scores revealed, that obese subjects improved postoperatively in food addiction (YFAS), food craving and pathological eating patterns (DEBQ emotional and external eating) ($p_s < 0.05$). No correlations between receptor availabilities and questionnaire scores were found except with STAI scores, which were negatively associated with preoperative [¹¹C]carfentanil BP_{ND} s in all ROIs ($r_s < -0.31$, $p_s < 0.04$).

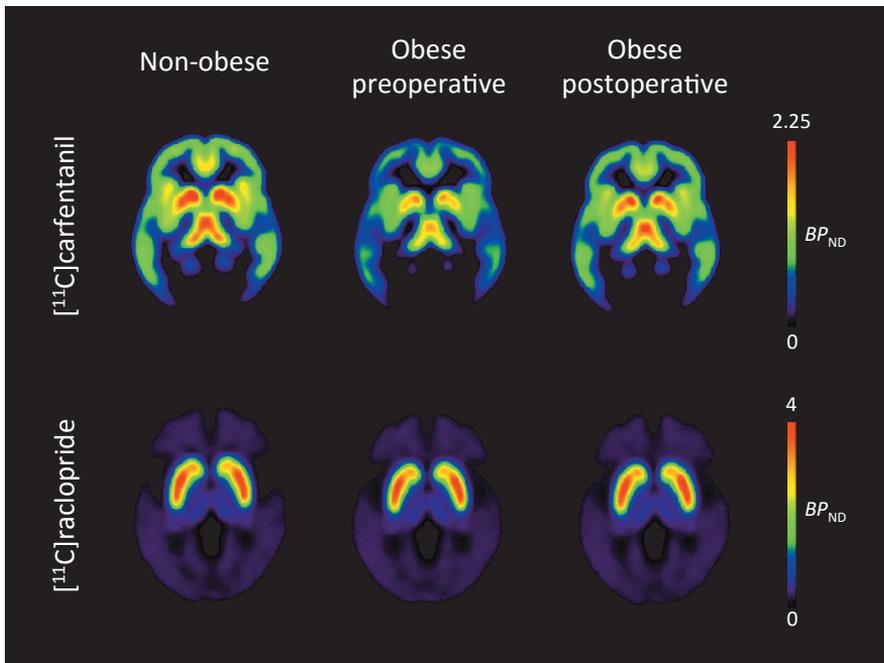


Figure 9. Preoperatively MOR availability was lower in the morbidly obese versus non-obese subjects. Bariatric surgery and weight loss however normalized the MOR availability (upper row) whereas D₂R availability was unaffected (lower row) (Original publication III).

5.4 Obesity is linked to cerebral atrophy and decreased white matter integrity (Study IV)

In this study, the differences in brain white and gray matter densities as well as white matter integrity between obese and non-obese subjects were investigated using VBM and DTI methods. In the VBM analysis, morbidly obese subjects had lower GM densities in right inferior frontal gyrus, left postcentral gyrus, inferior temporal gyri, right middle temporal gyri, temporal lobes, and occipital gyri (Figure 10). WM densities were decreased in the limbic regions and under superior and middle temporal lobes (Figure 10). Notably, GM and WM densities were not larger in morbidly obese versus non-obese controls in any brain region.

DTI analysis showed that morbidly obese versus non-obese subjects had lower FA values in corticospinal tracts, mamillary bodies, optic radiations, corpus callosum, and right inferior occipito-frontal fascicle, while lower MD values were found in uncinate fascicles and inferior occipito-frontal fascicles (Figure 11).

Anthropometric and metabolic variables were also correlated with the regional estimates of brain atrophy. BMI was associated with all the measures of brain atrophy (GM, WM, FA and MD) across the whole BMI range. In addition, percentage of fat correlated with the brain atrophy in most parts of the brain, while subcutaneous adipose tissue volume

associated negatively with most regional GM densities. Glycaemic status or blood pressure levels were not associated with any measures of cerebral atrophy.

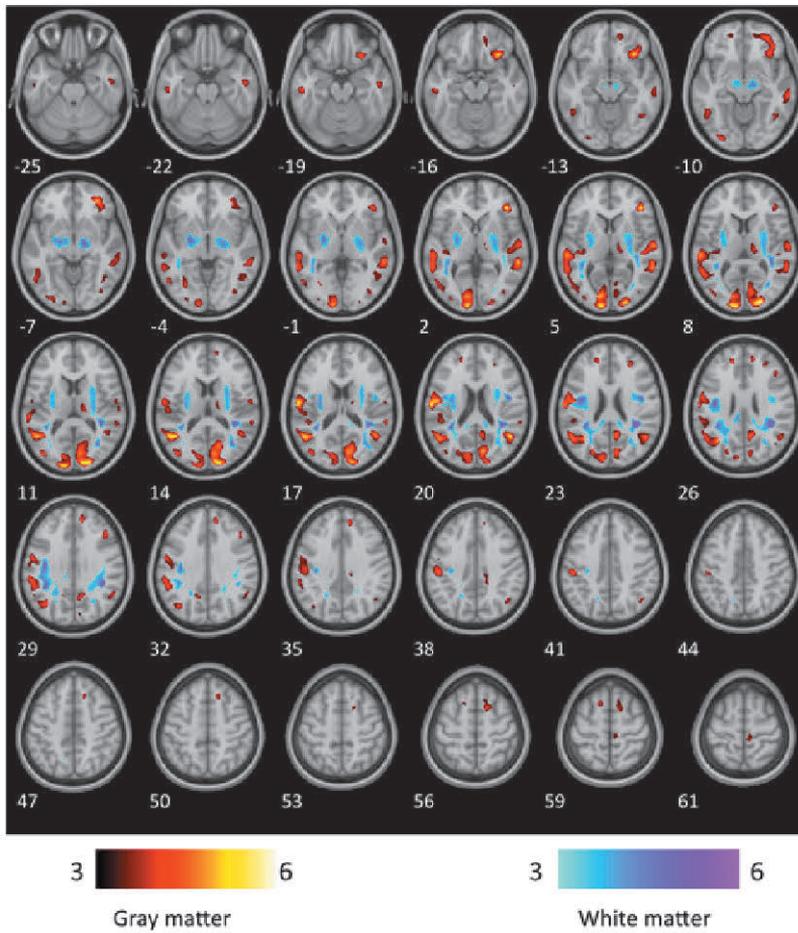


Figure 10. Brain regions that have decreased GM and WM densities in morbidly obese versus non-obese subjects (Original publication IV).

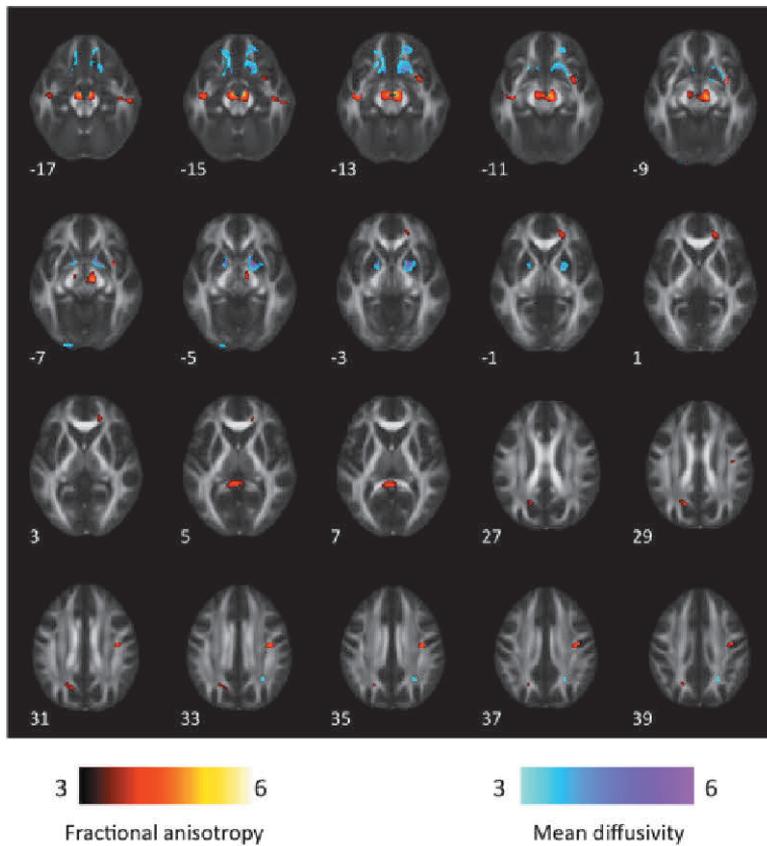


Figure 11. Brain regions that have decreased FA and MD densities in morbidly obese versus non-obese subjects (Original publication IV).

5.5 Bariatric surgery and weight loss recovers GM and WM atrophy in morbid obesity (Study V)

This study was performed in order to test whether bariatric surgery and concomitant weight loss would recover brain white and gray matter densities. VBM analysis was used to investigate i) GM and WM densities between non-obese subjects in the preoperative state and ii) the effect of surgery-induced weight loss on cerebral atrophy in the obese subjects.

Before the surgery, morbidly obese subjects had lower GM density in inferior orbitofrontal regions, frontal regions, and bilateral insula as well as temporal, occipital, and cerebellar regions (Figure 12). WM density was lower under the orbitofrontal gyri and in the midbrain/medulla (Figure 13).

Significant negative correlations were found between preoperative brain densities and

many metabolic variables such as fat percent, fat volumes, plasma lipids, and systolic blood pressure were found. Moreover, HDL cholesterol levels and physical activity associated positively with GM and WM densities in most areas.

Obese subjects' WM densities recovered significantly following the surgery-induced weight loss. The effect was observed globally in WM (Figure 13). GM recovery was found in smaller areas, mainly in occipital and inferior temporal regions (Figure 12).

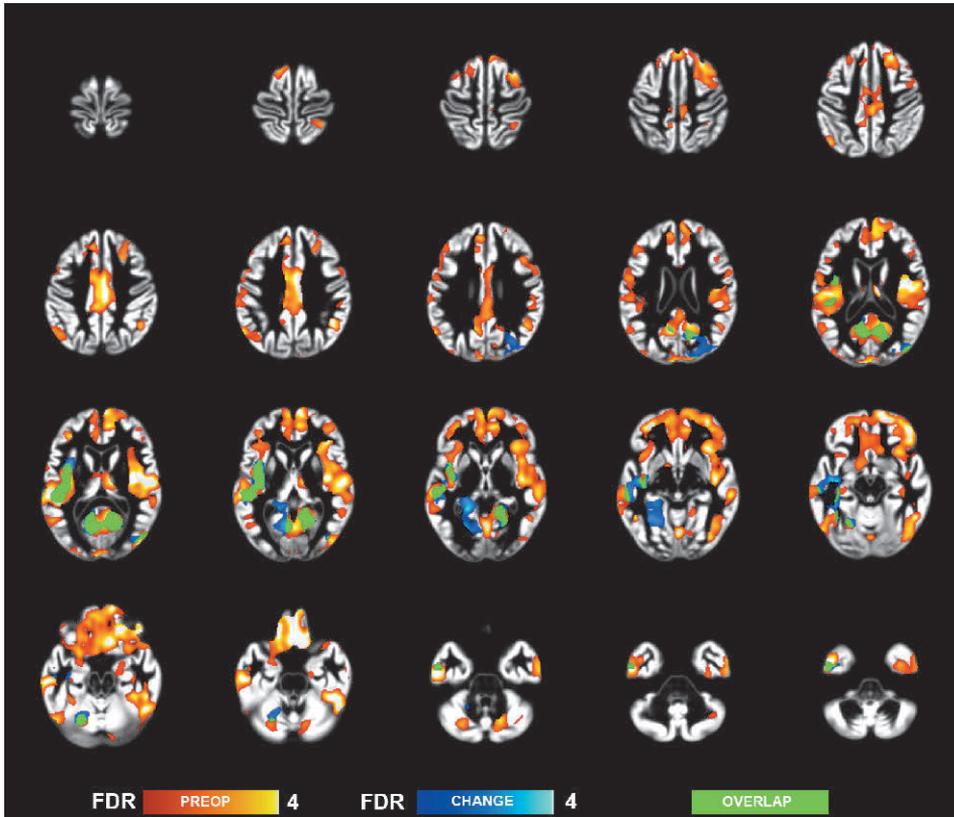


Figure 12. Brain regions with decreased GM density among obese subjects before the surgery (warm) and regions with increased GM density postoperatively (cool) (Original publication V).

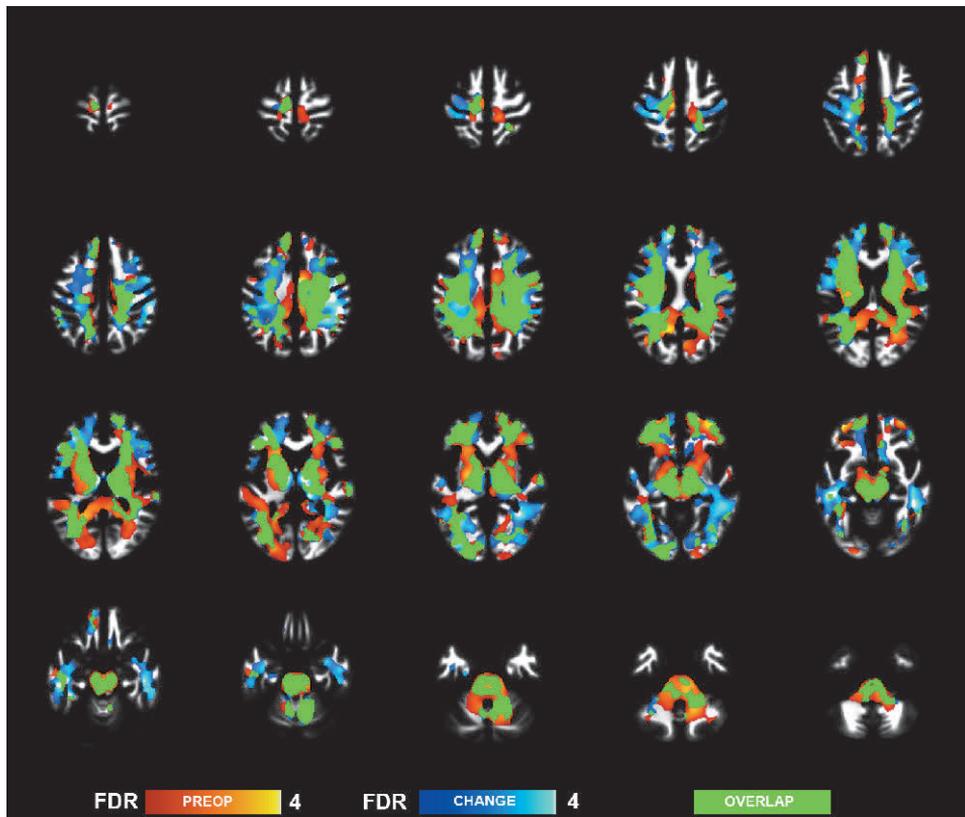


Figure 13. Brain regions with decreased WM density among obese subjects before the surgery (warm) and regions with increased WM density postoperatively (cool) (Original publication V).

6 DISCUSSION

6.1 Obesity is associated with opioidergic dysfunction

Main finding of this study was that morbidly obese subjects had lowered MOR but unaltered D₂R availability in many areas associated with the control of appetite. Decreased MOR availability was observed in the key region of the reward circuit (ventral striatum), regions implicated in emotional functioning (amygdala and prefrontal cortex), as well as those subserving homeostatic control (thalamus). Animal studies have demonstrated that endogenous opioid system is important in hedonic aspects of feeding (Pecina and Smith, 2010; Fields and Margolis, 2015), and pharmacological challenge studies have shown that both MOR antagonists and inverse agonists reduce human eating behaviour (Nathan et al., 2012; Cambridge et al., 2013). Opioidergic system also contributes to pleasurable sensations triggered by eating regardless of the type of food: even bland or aversive food can be rendered rewarding (Olszewski et al., 2011). The present study is however the first one to clearly point out that abnormalities of opioidergic neurotransmission are associated with human morbid obesity.

Early animal studies suggested that consuming palatable food elevates the level of β -endorphins in hypothalamus (Dum et al., 1983). More recent work in rodents has shown that palatable food consumption decreases MOR expression in ventral striatum, and withdrawal from palatable food increases it (Pitman and Borgland, 2015). In a similar vein, continuous intake of palatable food in obese individuals may increase the levels of cerebral β -endorphins and cause downregulation in MOR proteins to compensate for the perpetual overstimulation. This may lead to a vicious circle, where decreased amount of receptors or lower affinity of receptors lead to decreased net stimulation of opioidergic system, and in turn, force these individuals to eat more palatable food to get the normal hedonic response.

Human PET studies have shown that subjects with alcohol dependency have increased MOR availability in ventral striatum (Heinz et al., 2005), and also subjects with cocaine addiction have increased MOR availability even more widespread areas (Gorelick et al., 2005). Even though MOR system plays a significant role in both obesity and substance addiction, the underlying mechanisms seem to be different. Smoking did not have any significant affect to MOR availability in this study, which is in line with previous evidence employing PET with [¹¹C]carfentanil (Kuwabara et al., 2014).

Interestingly, a link between anxiety and MOR availability was also found. Endogenous opioid system is involved in neuromodulation of anxiety (Bodnar, 2008; Bowers et al., 2012), and it is known that affective states and stress can cause dynamic changes in the MOR system (Drolet et al., 2001; Zubieta et al., 2003; Ribeiro et al., 2005; Barfield et al., 2013). It is possible that overeating is partly maintained by inability to control emotional arousal states such as anxiety. Thus, obese subjects may use food to alleviate the sensation of anxiety. It has previously been shown that subjects with mood disorders have often

diets high in sugar and fat (Davison and Kaplan, 2012). Reduction of negative affective states may partly arise from overeating, which can also affect to MOR system.

Somewhat surprisingly, no differences between D₂R availabilities in morbidly obese versus non-obese subjects were observed. This contradicts some previous imaging studies (Wang et al., 2001; de Weijer et al., 2011), yet present data are in line with majority of reports (Haltia et al., 2007b; Haltia et al., 2008; Steele et al., 2010; Eisenstein et al., 2013; Guo et al., 2014). Different results in PET studies might be related to, for example, the severity of obesity in the subjects, but also different feeding conditions. These PET scans were performed two hours after last meal. D₂R availability is likely very sensitive to feeding status (Small et al., 2003), although intravenous glucose administration does not affect on D₂R availability, possibly because of overtaken gut hormone activation. Sensitivity of D₂R availability to eating was also speculated in a recent work, where increased D₂R availability was found after 8,5 hours fasting period (Dunn et al., 2012). Authors hypothesized that this might be due reduced dopamine levels of fasting state. In the study showing the greatest effect between BMI and D₂R availability, feeding status of subjects remains indefinite (Wang et al., 2001). Moreover, in the same study, subjects had very high BMI (mean 51) and were completely unmedicated and free of chronic diseases.

In Study II, striatal opioid and dopamine systems were found to be tightly coupled in non-obese but not in obese subjects. In other words, the more MOR the subjects had, the higher were their D₂R levels. Interaction was strongest in ventral striatum, but significant also in dorsal caudate. Interrelated expression between these receptors has not been previously characterized in human reward circuit. Some evidence from rodent studies exists that MOR and D₂R are expressed in same striatal neurons (Ambrose et al., 2004; Margolis and Hjelmstad, 2014). The interaction between these receptor systems is likely crucial in regulating appetite because it breaks down in ventral striatum in the obese subjects, while association in dorsal caudate remains intact. This might explain unaltered D₂R levels in obesity: although obesity-dependent dysfunction in dopaminergic system is shown in numerous animal studies, it may be mediated through MOR-dependent mechanisms without having any effect on the actual amount of D₂R protein. Even if the amount of D₂R protein is not altered in obesity, decoupling of MOR and D₂R in ventral striatum may cause altered dopaminergic functions.

6.2 Bariatric surgery and weight loss recovers the opioidergic dysfunction in the brain reward circuit

Bariatric surgery normalized MOR expression in the morbidly obese subjects, confirming that there exists a link between weight changes and MOR system. This is the first-ever demonstration of the weight loss dependent changes in MOR signalling in humans. This fits with animal studies showing that MOR expression increases after withdrawal from palatable and high-fat diet has been observed (Pitman and Borgland, 2015). Normalization of MOR in the reward circuit after weight loss suggests that excessive eating may lead to perpetual overstimulation of the MOR system, which subsequently causes MOR downregulation. This may lead to overeating in order to get compensate for lowered hedonic impact of food intake. However, downregulated MOR can be brought back to the normal levels, which may also impact eating behaviour. In line with this, increase in MOR

availability was paralleled with lowered self-reported food craving as well as emotional and external eating. Behaviourally this is in line with previous studies, that show improved satiety and lowered appetite after bariatric surgery (Morinigo et al., 2006; Karamanakos et al., 2008), which might be due to change in gut hormones such as ghrelin (Munzberg et al., 2015). Interestingly, both natural food reward and systemic ghrelin administration activates MORs. Ghrelin also influences on dopamine release in ventral striatum (Kawahara et al., 2013). This shows a possible link between gut hormone alterations and MOR changes after bariatric surgery.

It is however possible that healthier eating habits do not arise only from the recovery of MOR availability. Reduced appetite after bariatric surgery may partly be due the change in gastrointestinal hormone secretion (Schmidt et al., 2013). Based on this study, it is not possible to fully differentiate the effect of bariatric surgery *per se* versus weight loss on MOR system. However, it was recently shown, that also weight loss caused by low-calorie diet can cause similar increase of MOR availability as observed here. Obese men without binge-eating habits have decreased MOR availability but this is partly recovered after 15 % weight loss (Burghardt et al., 2015). This study had only a few subjects (7 obese and 7 controls), but they were scanned both in fasting and fed states. Normal-weight men had increased MOR availability after a standard meal, but within the obese subjects the activation of MOR system was lower. Based on this study, obesity seems to affect both receptor density and endogenous opioid release. This suggests that the surgical operation itself is unlikely to underlie the normalization of the MOR system, and that weight loss and altered eating habits play a major role here.

It should be noted that also other neuroreceptor systems might be involved in the normalization of appetite after bariatric surgery. Recently, changes in the serotonin receptor binding were observed after Roux-en-Y gastric bypass (RYGB) operation in obese subjects (Haahr et al., 2015), which suggest that the control of appetite involves the serotonergic system as well. To make the picture even more complicated, MOR system is interacting with endocannabinoid system in food intake (Lockie et al., 2011). All in all, many homeostatic and neuroreceptor systems play role in appetite control, and subtle changes in these may have intense affects on weight balance.

Increased substance abuse has been reported among patients who have undergone bariatric surgery (Suzuki et al., 2012), and a recent study with rats showed significantly increased morphine self-administration after Roux-en-Y gastric bypass (RYGB) operation (Biegler et al., 2015). Furthermore, rodent studies have shown increase in alcohol reward (Hajnal et al., 2012) and increase in alcohol self-administration (Polston et al., 2013) after RYGB. It is possible that this is at least partly due to changes in opioidergic signalling, which was also observed in this study. Individuals undergoing RYGB may compensate lacking food-driven hedonia (restricted by RYGB) by stimulating the MOR system with drugs of abuse (Volkow and Wise, 2005). However, in this study none of the obese subjects reported any increase in substance abuse.

No postoperative change in the D₂R availability was observed. This is line with an earlier SPECT study that did not find any change in D₂R availability after weight loss (de Weijer et al., 2014), although two other PET studies with significantly smaller samples have shown contradictory results, one increased (Steele et al., 2010) and other decreased (Dunn et al., 2010) D₂R availability. The follow-up period in all these studies was 6 weeks, which does not make these studies fully comparable to our study. However, a recent SPECT study has observed significant increase in D₂R availability after two years from

bariatric surgery (van der Zwaal et al., 2016), which implies that changes in D₂R availability may occur slowly over time. Although it was not possible to detect any change in D₂R availability in Study III, dopaminergic system is likely extremely important in the function of the reward circuit, especially in wanting and craving, but this cannot be seen with PET imaging. Changes in the interaction between D₂R and MOR might explain some of the changes in the eating pattern, but this remains to be investigated.

6.3 Obesity has a profound impact on brain anatomy and integrity but this is reversed after bariatric surgery

Obesity was associated with lowered GM densities in wide regions of the brain. This accords with previous studies, which have showed a clear inverse association between BMI and GM densities. Studies IV and V revealed lowered focal GM densities basically in the same areas than in most previous studies. (Pannacciulli et al., 2006; Gunstad et al., 2008; Taki et al., 2008; Ho et al., 2010; Raji et al., 2010; Cazettes et al., 2011; Horstmann et al., 2011; Bobb et al., 2014; Debette et al., 2014; Janowitz et al., 2015). No difference between subject sex and atrophy was seen, which contradicts some previous studies (Taki et al., 2008). Based on Studies IV and V, both sexes seem to be at risk to obesity-related brain atrophy.

WM was also preoperatively decreased in obese subjects, but in more limited regions. WM reduction has also been showed earlier (Raji et al., 2010), although contradictory studies exist too (Haltia et al., 2007a). This finding was corroborated with the DTI analysis, which revealed loss of integrity in more specific parts of the brain. Decreased FA and MD values were found in cortical and limbic areas of the brain. Lower FA refers to axonal degeneration and demyelination, which is in line with VBM results. Lower FA values are observed, for example, in multiple sclerosis, which is a demyelinating disease (Roosendaal et al., 2009). Lower MD values found in uncinate fascicles and inferior occipito-frontal fascicles are more difficult to interpret. High MD is a measure of membrane dysfunction; lower values suggest higher myelination and denser axonal packing. However, low MD values can be interpreted as dysfunctional energy metabolism, which can explain the observed changes, given that obesity is associated with altered glucose metabolism (Tuulari et al., 2013). Low MD values are seen, for example, in ischemic stroke (Bhagat et al., 2008).

Obese subjects' grey matter density was significantly lower in cortical areas that govern executive function, long-term memory, vision processing and somatosensory functions. It is possible that these structural changes could partly underlie altered reward processing and overeating in obesity. Also previous studies have established that obese individuals have structural changes in the regions that control feeding behaviour (Pannacciulli et al., 2006), but the importance of these structural findings is elusive.

In both Studies IV and V, preoperatively observed brain abnormalities in the obese subjects correlated with body fat percentage, and lowered GM densities also correlated with the volume of subcutaneous fat. It is thus likely that some of the changes in brain structure are due to low-grade systemic inflammation caused by adipose tissue (Vachharajani and Granger, 2009; Gregor and Hotamisligil, 2011; Lumeng and Saltiel, 2011). Association

between lowered brain integrity and inflammation has been observed before in overweight and obese subjects (Cazettes et al., 2011). White adipose tissue is known to produce many different inflammatory molecules that can cause damage to brain tissue (Debette et al., 2010; Aguilar-Valles et al., 2015). These inflammatory markers such as C-reactive protein and interleukin-6 are significantly reduced after bariatric surgery (Rao, 2012), which is beneficial to brain health.

Using a larger sample in Study V, clear associations were established between cerebral atrophy and previously suggested risk factors for atrophy, such as hypertension (Taki et al., 2004; Enzinger et al., 2005), diabetes (Korf et al., 2007) and abnormal cholesterol profile (Cohen et al., 2011). HDL and exercise might have a protective role in brain atrophy while high levels of triglycerides are linked to brain density reductions. Risk factors for brain atrophy are thus quite similar than those for atherosclerosis. This emphasizes the need for strict glycaemic control as well as anti-hypertensive and anti-cholesterol therapies also for those obese patients who do not seem to achieve significant results in weight loss. Additionally, physical activity can be recommended to obese patients to protect brain from deterioration.

Significant recovery in WM densities after bariatric surgery was observed, which is probably due to reduction in low-grade inflammation. This is in line with one prospective study, which showed that lowered WM densities – rather than lowered GM densities – are secondary to weight gain (Yokum et al., 2012). GM density increase was also observed, but its extent was more limited. It is possible that six months is a too short interval to observe changes in GM. Thus, it is too hasty to predict whether some of the alterations in GM have preceded weight gain. It has to be pointed out, that some of the decreased focal GM densities in the cross-sectional analyses were found in areas implicated in reward processing. For example, there was reduction in the density of orbito-frontal areas, which have previously been linked to hedonic processing (Kringelbach, 2005). Some researchers have indeed proposed that structural alterations in hedonic and homeostatic systems contribute significantly to weight gain and eating behaviour (Horstmann et al., 2011). Longer follow-up studies with more intermediate scans are thus needed to reveal whether more widespread GM recovery occurs following weight gain, and also to establish the trajectories of the grey and white matter density recovery.

6.4 Clinical implications

The dysfunction of endogenous opioid system in the reward circuit is a key component underlying overeating, and thus a feasible target for pharmacological and behavioural interventions. This has already been noted in pharmacological studies. For example, MOR antagonist naltrexone reduces pleasantness of food in human subjects (Murray et al., 2014). Even though naltrexone therapy alone does not lead to significant weight loss, more promising results are obtained when it is coupled with bupropion (a dopamine and norepinephrine re-uptake inhibitor) (Lee and Fujioka, 2009; Greenway et al., 2010; Smith et al., 2013; Billes et al., 2014). This might be due to tight coupling of MOR and D₂R, as shown in Study II. Moreover, the success of the combination therapy underlines the complex pattern of neurotransmitter networks underlying overeating, and suggests that both aspects of reward functions – *wanting* and *liking*, processes mediated by dopaminergic

and opioidergic systems, respectively (Berridge and Kringelbach, 2015) – have to be taken care of in order to treat obese patients. Although no obesity-dependent changes was observed in dopaminergic system *per se* using PET with [¹¹C]raclopride, previous animal studies strongly support the relevance of dopaminergic pathways in obesity (Baik, 2013). However, the dopamine-centered reward deficiency theory of food addiction is likely obsolete, which is also supported by a recent meta-analysis (Benton and Young, 2016). Obesity and overeating can also affect dopaminergic signalling via the function of DATs, which were not investigated in these studies. Of note, some of the effects driven by dopaminergic system can be mediated through opioid system, as close interaction with these systems was shown in Study II.

It should be noted that not all the patients benefit from the anti-obesity drugs. Furthermore, behavioural interventions are often inefficient. Bariatric surgery needs to be used with certain obese patients who have failed in non-invasive weight loss strategies. Surgical procedures cause long-term weight loss and also reduce mortality (Sjostrom et al., 2007). However, bariatric surgery involves significant risks and is quite expensive (total cost around 10 000 € per operation in Finland during the year 2015). Thus, the price per one kilo's weight loss is significantly higher than successful weight loss using behavioural or pharmacological therapies. This is why the selection of subjects to undergo a bariatric surgery must be strict. Nonetheless, due to the prevalence of obesity, cheaper and more effective treatments are urgently needed.

Obesity has a unique neurochemical profile in the brain reward system, which is not entirely shared by addictive disorders and substance abuse. Characterizing obesity merely as an addiction would thus be oversimplification. Abuse of drugs causes direct neurochemical effects to reward circuit, which in turn leads to addiction, without any natural homeostatic mechanisms involved. Thus, obese subjects should not be treated just like patients with addicted disorders. Although there were similar changes in the opioid system than some opioid users have (Koch and Holtt, 2008), physiological regulation of feeding as well as the necessity of regular food intake makes obesity a much more complex problem.

Many metabolic variables were associated with brain atrophy among obese. For example, cholesterol profile has a profound impact on brain atrophy in obese. This alludes to more intensive anti-cholesterol therapies to protect brain. Weight loss due to bariatric surgery was found to have beneficial effects to brain structure even in relatively short follow-up period. For example, obesity increases risks for neurodegenerative disorders such as Alzheimer's and Parkinson's diseases (Kivipelto et al., 2005), and weight loss protects against these diseases (Ashrafian et al., 2013). In a large prospective cohort study, BMI had a strong negative correlation with cognitive performance, and higher baseline BMI also associated with more prominent cognitive decline in the future (Cournot et al., 2006). Especially male subjects seem to be in risk for obesity-related cognitive impairment (Elias et al., 2005). Bariatric surgery might thus be very beneficial for countering the obesity-induced cognitive decline. There is clear evidence that weight loss after surgery improves cognitive functions and memory significantly (Miller et al., 2013; Stanek and Gunstad, 2013; Alosco et al., 2014b). All in all, weight loss is very advantageous in protecting the brain from cognitive decline. Moreover, also moderate physical exercise such as walking can significantly protect from brain volume reductions and cognitive impairment (Erickson et al., 2010; Ho et al., 2011), which was also seen in Study V.

When treating patients with obesity, the diversity of neural mechanisms behind the control of appetite should be kept in mind. Individual differences might also have an important role in eating; there might even be different neural or psychological phenotypes causing obesity, which we are not yet aware of. For example, studies utilizing fMRI have shown differences between obese individuals with and without binge eating disorder (Balodis et al., 2013b; Balodis et al., 2013a). In the future, more personalized therapies may come into picture when treating different patients. Cognitive reappraisal strategies may be effective to some obese subjects (Yokum and Stice, 2013), some may benefit from behavioural therapies while others must be operated using surgical procedures. Even video games may turn helpful in this task, knowing that they can directly affect at least the dopaminergic system (Koepp et al., 1998).

6.5 Limitations of the studies

PET studies have certain limitations. In data analysis, using BP_{ND} as a measure of receptor binding, changes in receptor availability may be due to changes in the amount of actual receptor protein, receptor affinity, or the amount of endogenous neurotransmitter occupancy in the receptor proteins. Moreover, in the PET studies only a D₂R antagonist [¹¹C]raclopride was used, while a D₂R agonist ligand could be more sensitive for detecting changes in receptor availability among subjects with moderate BMI (Caravaggio et al., 2015). Moreover, we measured only baseline receptor availabilities, and did not measure the effects of eating on receptor system activity, which may affect both MOR (Burghardt et al., 2015) and D₂R availabilities (Small et al., 2003).

In the study III, it was not possible to differentiate the combined effects of postoperative weight loss and altered gut anatomy and function. Altered neuroreceptor availability may be due to the changes in gut hormones but also due to reduced intake of palatable foods. Further studies are needed to elucidate the sole effect of weight loss due to altered energy intake on MOR availability by comparing the effects of weight loss by surgery versus dieting. However, a recent study using conventional weight loss manipulation by dieting suggests that the changes in MOR availability are due to weight loss, not due to gastrointestinal changes (Burghardt et al., 2015). Some patients may start gaining weight later than six months from the bariatric surgery (Cooper et al., 2015) suggesting that longer follow-up studies are needed. Based on preoperative receptor availabilities, future weight gain might be predicted, which opens up new possibilities for research.

Optimally, to get a more complete picture of causal relationships between obesity and brain changes, prospective studies concentrating on developmental trajectories should be performed. Weight loss seems to normalize MOR availability but we do not know whether weight gain decreases it. However, using PET with follow-up studies is problematic due to high radiation doses. MRI follow-up studies are less problematic, and these could be combined with extensive metabolic data to understand the factors behind changes appeared in VBM and DTI. Furthermore, the actual molecular mechanisms behind the increased MOR availability following weight loss still remain unknown, and may be achievable only using translational studies with rodents and humans.

To avoid high radiation doses caused by a longitudinal PET study such as this, the same amount of radioactivity was injected to both obese and non-obese subjects. Due to smaller count rates in the obese subjects' brains, a theoretical risk of underestimation of the SRTM derived BP_{ND} remains. The risk may be more prominent with high-resolution research PET scanners using iterative reconstruction, but less crucial with more conventional whole body PET scanners such as GE Healthcare Discovery 690 PET/CT, which was used in these studies. However, to further ensure that the SRTM estimated BP_{ND} s were accurate, the injected amounts of radioactivity per weight (kg) were correlated with MOR and D₂R availabilities in all ROIs, but no correlation was found. Moreover, normalization of MOR availability postoperatively did not depend on the amount of lost weights, indicating that underestimation of BP_{ND} s is unlikely. Our results also resemble the findings of a recent study (Burghardt et al., 2015), which used [¹¹C]carfentanil with bolus and infusion method as well as iterative reconstruction.

The study groups also limit the generalizability of the findings. In the PET studies, only female subjects were studied, and the results may not be generalizable to male subjects. In the MRI studies, majority of the subjects were also females. Although no gender differences were observed, the groups could have been more balanced. Moreover, morbidly obese subjects were compared with non-obese controls. Studying also subjects with moderate levels of obesity (e.g. BMI between 25 and 35 kg/m²) could have revealed the critical 'tipping point' in BMI after which brain anatomy and function begins to alter.

6.6 Future directions

The prevalence of obesity is dramatically increasing and there is urgent need for efficient therapies. Obesity is highly expensive for the society, especially due to the secondary chronic diseases. The obesity-linked sequelae such as type 2 diabetes also reduce person's life expectancy and quality of life. It is plausible that in order to tackle the obesity epidemic, many different therapies must be combined.

Pharmacological therapies against obesity have emerged over the years. However, most anti-obesity drugs have adverse side effects, and this has forced the medical companies to withdraw them from markets. Together with naltrexone and bupropion combination therapy, homeostatic mechanisms of food intake may however provide a feasible target for obesity medication. The newest and the most promising anti-obesity drug is liraglutide, a GLP-1 receptor agonist, which is already sold also in the European markets. It is clearly more efficient for weight loss than orlistat, and improves many cardiovascular risk factors (Astrup et al., 2012; Vilsboll et al., 2012; Pi-Sunyer, 2015). GLP-1 binds to GLP-1 receptors located in the areas related to appetite and reward, but it has also direct effect on mesolimbic neurons in ventral tegmental area (Skibicka, 2013; Baggio and Drucker, 2014). However, to achieve significant weight-loss, efficient life-style interventions should be combined with GLP-1 receptor agonists. Recently, an animal study showed that a drug affecting three gut hormone receptors (GLP-1, glucose-dependent insulinotropic polypeptide and glucagon) causes notable reduction of weight (Finan et al., 2015). In the future, we need more data how these gut hormones affect brain's appetite control.

Opioidergic and dopaminergic systems play a role in governing the motivational and rewarding aspects of feeding and the choice of food. This project shed light on the opioidergic dysfunction in obesity, but also the close interaction between these two neurotransmitter systems was shown in Study II. Molecular basis of this interaction – and the disruption of the interaction among obese - needs further verification using animal work. In addition, more studies about the associations between homeostatic regulation of appetite and reward circuit should be performed to get the comprehensive picture of the human appetite control. Gut hormones are known to have direct effect to dopaminergic system; for example, leptin and insulin inhibit dopaminergic system while ghrelin activates it (Palmiter, 2007; Kenny, 2011). Furthermore, the interaction between ghrelin and MOR system in weight loss should be further investigated, because promising new data has been observed (Kawahara et al., 2013). Combining different modalities of brain research, such as PET and fMRI, might be proven successful in this task, although few studies exist yet (Dougherty et al., 2008) Finally, volitional appetite control (Tuulari et al., 2015) and insulin resistance (Heni et al., 2015) also play a role in weight regulation. For example, nasal insulin influences hunger in male subjects (Kullmann et al., 2015). The interaction between gut hormones and brain reward systems needs further research to find implications for management of obesity.

It is unlikely that we can achieve this goal by studying human subjects only. Intensive translational research combining animal studies to human neuroscience studies will lead us closer to the understanding of appetite control. Within this project, it has been shown that obesity has adverse effects on brain function and structure. The actual mechanisms behind these alterations as well as the mechanisms behind the positive change in structure and function after bariatric surgery still remain unclear and should be addressed in future research.

7 CONCLUSIONS

This multimodal brain imaging project revealed that obesity and weight loss influence brain structure and the neural circuits responsible for reward processing in obesity. Although obesity is fundamentally caused by an imbalance between energy gain and energy expenditure, it was shown for the first time that the dysfunction of the endogenous opioid system inside the reward circuit is intimately linked to human obesity.

It is critical to understand that the adverse changes in the opioidergic system may lead to continuance of pathological eating habits. It is now clear that obesity has adverse effects on brain structure as well, but this can be reversed by bariatric surgery and following weight loss. Results showed in this thesis suggest that the cerebral changes associated with obesity are related to the obese phenotype and have developed after weight gain, rather than representing stable neural characteristics of increased propensity to gaining weight. Consequently, obese individuals can affect to their brain health in a positive way by losing weight.

The reward system in mammals has developed by evolutionary processes in such conditions, where food has been scarce. Thus, it has been crucial that an animal is willing to find food and willing to eat it. Nowadays, when especially palatable energy-dense food is abundant and easily obtainable, it is even surprising that many people remain normal-weight. Findings presented in this thesis narrow the gap between previous human and animal studies on the neural architecture of the reward circuit and its dysfunction in obesity. Based on these findings, it is too simplistic to consider common metabolic obesity as "food addiction". Although the motivation to eat is likely processed via same routes in the reward circuit than the motivation to use drugs of abuse, overeating comprises a much more complex problem. Moreover, its neurobiological profile is unique and distinct from that observed in other addictive disorders. In obesity, hedonic aspects of energy-dense food distort the basic need for energy to survive.

Finally, regulation of appetite occurs via multiple mechanisms. It is likely that overeating is caused by dysfunction of all these systems, and in the future, with the help of the studies presented in this thesis, we are hopefully a little bit closer to assembling the complex picture of appetite control and the mystery of obesity. The findings described in this thesis may help to develop new clinical treatments for obesity. Understanding the changes in the reward-controlling systems among obese subjects will provide information for future pharmacological interventions as well as effective behavioural and psychological interventions for obesity, and thus have a major effect on the national health.

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